

## **Lecture 11**

# **Biopotential Amplifiers: the Electrocardiogram**

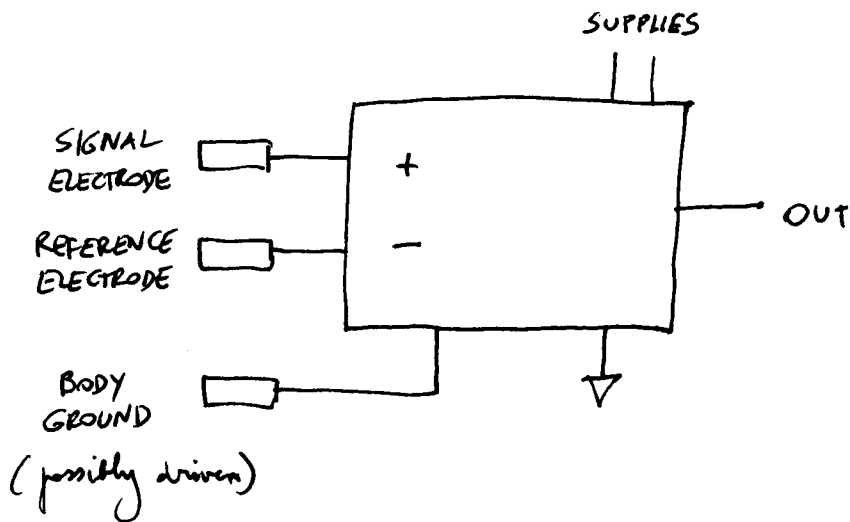
### **References**

Webster, Ch. 6 (Sec. 6.1-6.2) and Ch. 4 (Sec. 4.6 Review).

<http://en.wikipedia.org/wiki/ECG>

# BIO POTENTIAL AMPLIFIERS

Chap. 6



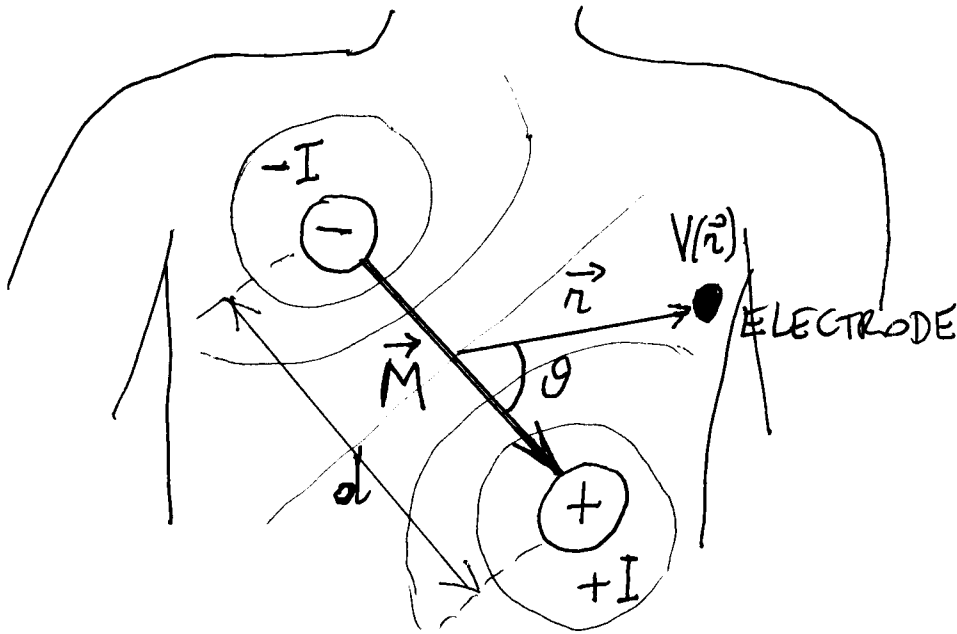
Requirements:

- high gain (differential)
- high input impedance
- input protection ( $\rightarrow$  input diodes)
- high rejection of artefacts and interference to the signal
  - high common-mode rejection (low common-mode gain)
    - $\rightarrow$  matched electrode impedances
    - $\rightarrow$  driven right leg (DRL) active ground
  - high interference rejection
    - $\rightarrow$  shielding
    - $\rightarrow$  filtering matched to frequency range of signal

Example: ECG biopotential amplifier

(Sec. 6.2; also Sec. 4.6 revisited)

# ECG revisited : DIPOLE MODEL



$\vec{M}$  : CARDIAC VECTOR : an approximate linear model of the effect of placement of the electrode at  $\vec{r}$ , relative to the current dipole of the heart at time  $t$ , on the measured potential :

$$V(\vec{r}, t) \approx \vec{M}(t) \cdot \vec{r} \quad \text{DOT PRODUCT}$$

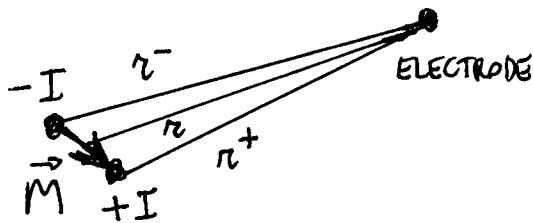
CARDIAC VECTOR  
as a function of  
time
ELECTRODE  
POSITION  
(fixed)

$$= \|\vec{M}\| \cdot \|\vec{r}\| \cdot \cos \theta$$

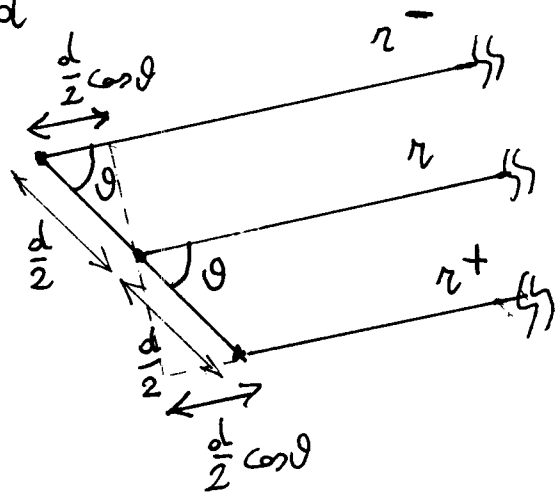
magnitude
angle

The cardiac vector model is valid only for large, and constant,  $|\vec{r}|$  relative to the dipole displacement  $d$ :

$$|\vec{r}| = r \gg d$$



Zoom



$$V(\vec{r}, t) = \frac{I(t)}{4\pi\sigma} \left( \frac{1}{r^+(t)} - \frac{1}{r^-(t)} \right) \quad \text{and} \quad \begin{cases} r^- \approx r + \frac{d}{2} \cos\theta \\ r^+ \approx r - \frac{d}{2} \cos\theta \end{cases}$$

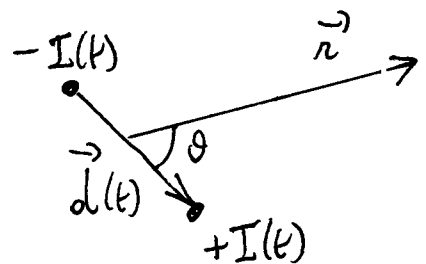
$$\frac{1}{r^+} - \frac{1}{r^-} \approx \frac{1}{r - \frac{d}{2} \cos\theta} - \frac{1}{r + \frac{d}{2} \cos\theta} = \frac{1}{r} \left( \frac{1}{1 - \frac{d}{2r} \cos\theta} - \frac{1}{1 + \frac{d}{2r} \cos\theta} \right)$$

$$\approx \frac{1}{r} \left( \left( 1 + \frac{d}{2r} \cos\theta \right) - \left( 1 - \frac{d}{2r} \cos\theta \right) \right) = \frac{d}{r^2} \cdot \cos\theta$$

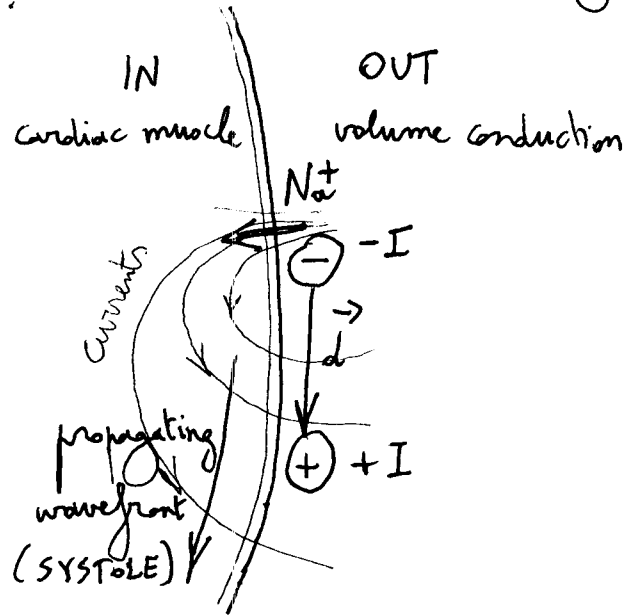
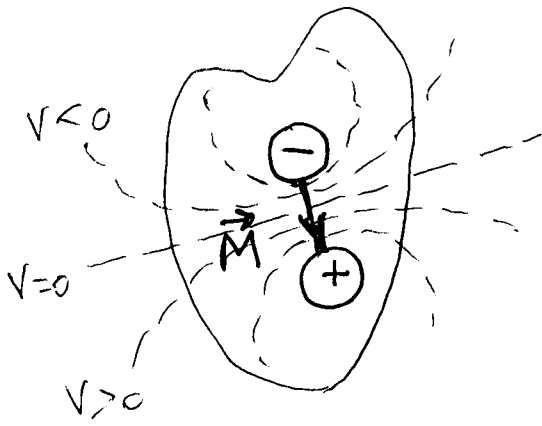
$$\left( \frac{1}{1+\epsilon} \approx 1-\epsilon \text{ for } |\epsilon| \ll 1 \right)$$

$$\Rightarrow V(\vec{r}, t) \approx \frac{I}{4\pi\sigma} \cdot \frac{d}{r^2} \cdot \cos\theta = \underbrace{\frac{I}{4\pi\sigma} \cdot \frac{d}{r^3}}_{|\vec{M}|} \cdot r \cdot \cos\theta = \vec{M}(t) \cdot \vec{r}$$

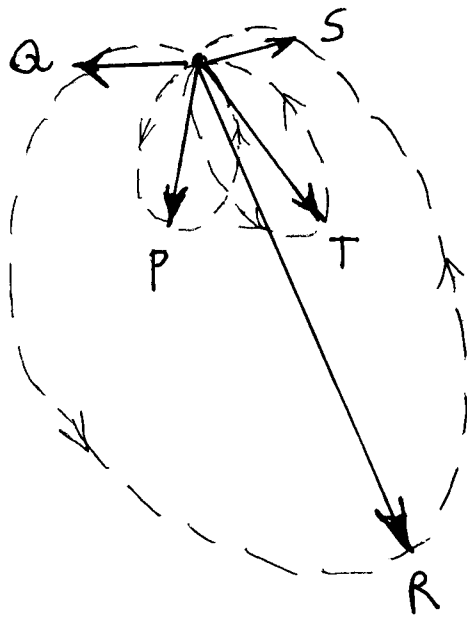
$$\Rightarrow \vec{M}(t) = \frac{I(t)}{4\pi\sigma} \cdot \frac{\vec{d}(t)}{r^3}$$



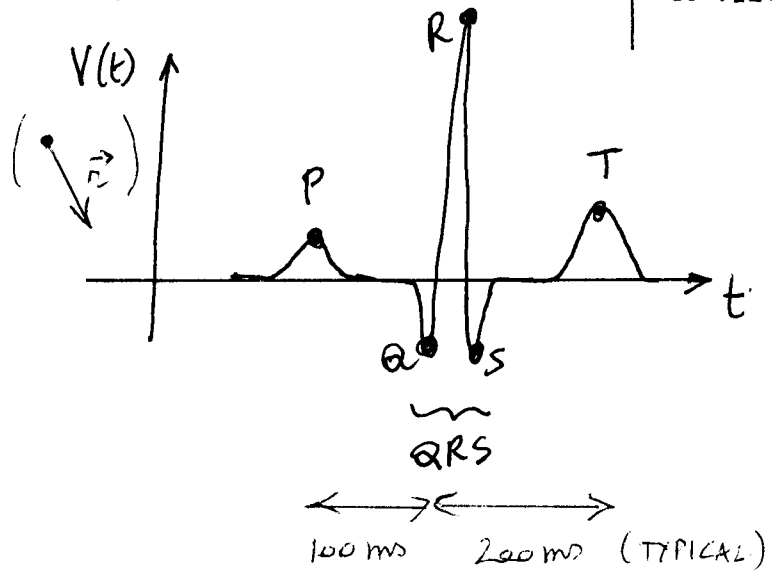
The cardiac vector varies with time over the cardiac cycle,  
 e.g. ventricular depolarization:



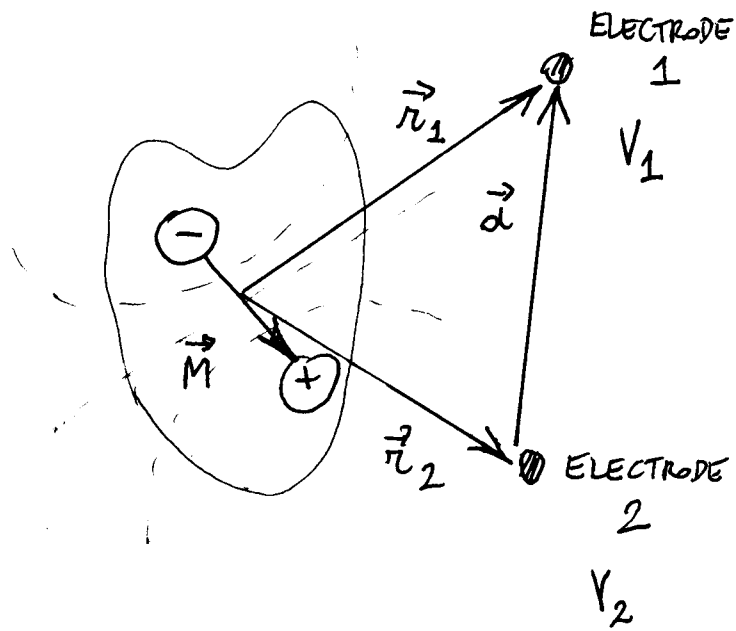
$\vec{M}(t)$ : traverses three main loops:



P-wave : atrial depolarization  
 QRS-complex : ventricular depolarization  
 T-wave : ventricular repolarization



ECG "leads": differential electrode configurations across the body, each picking up different projections of the cardiac vector time waveform



$$\vec{\alpha} = \vec{r}_1 - \vec{r}_2$$

LEAD VECTOR

$$V_{\alpha} = V_1 - V_2$$

LEAD VOLTAGE (DIFFERENTIAL)

$$V_{\alpha} = V_1 - V_2 = \vec{M} \cdot \vec{r}_1 - \vec{M} \cdot \vec{r}_2 = \vec{M} \cdot (\vec{r}_1 - \vec{r}_2)$$

$$\Rightarrow V_{\alpha} = \vec{M}(t) \cdot \vec{\alpha}$$

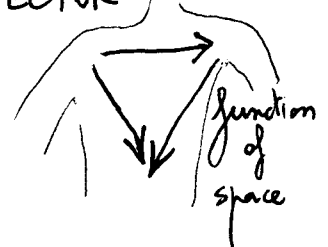
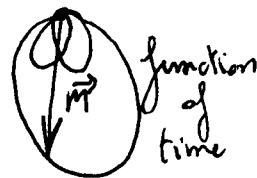
LEAD VOLTAGE

CARDIAC VECTOR

(DOT)

LEAD VECTOR

measured by a differential amplifier



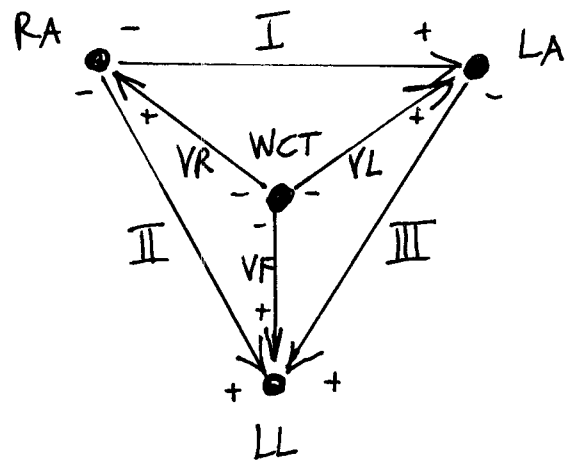
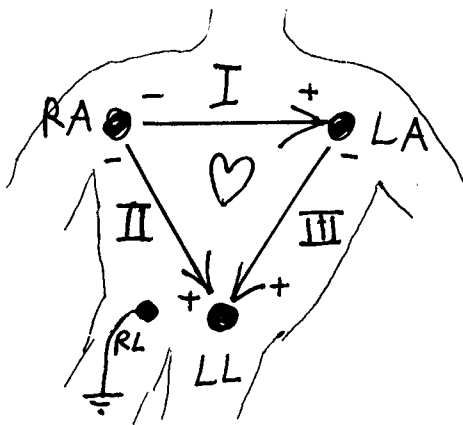
NOTE: this only works when  $\|\vec{r}_1\| = \|\vec{r}_2\| = r$ !

otherwise the two cardiac vectors are different

— Frontal plane : EINTHOVEN'S TRIANGLE

4 electrodes:  $\left\{ \begin{array}{l} RA \text{ right arm} \\ LA \text{ left arm} \\ LL \text{ left leg} \\ RL \text{ right leg} - \text{active grounding reference} \end{array} \right.$

Placed anywhere on the arms and legs since no current should flow through these.



6 leads in the frontal plane from these 3 (4) electrodes:

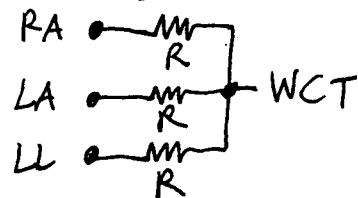
I : LA - RA	VR : RA - WCT
II : LL - RA	VL : LA - WCT
III : LL - LA	VF : LL - WCT

(vector differences)

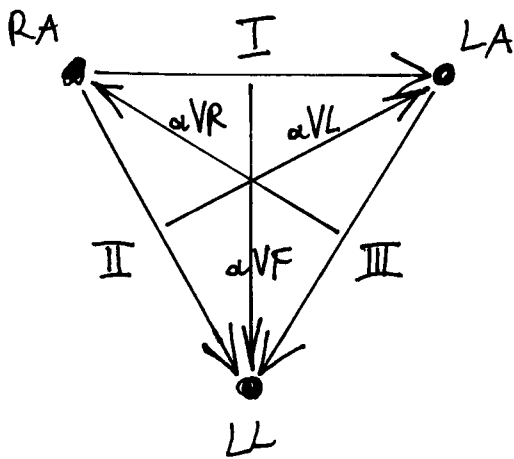
where WCT is the WILSON CENTRAL TERMINAL :

virtual ground reference at the center of the triangle

$$WCT = \frac{1}{3} (RA + LA + LL)$$



"Augmented" leads: alternative constructions of the VR, VL and VF leads with magnitude closer to the I, II, III leads:

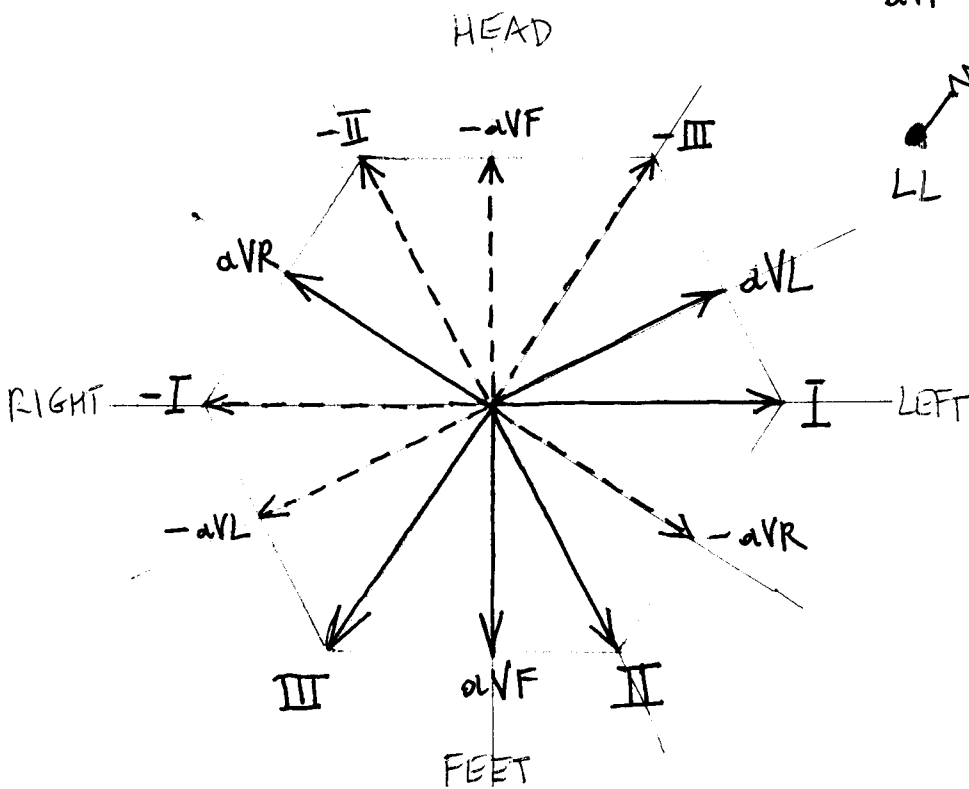
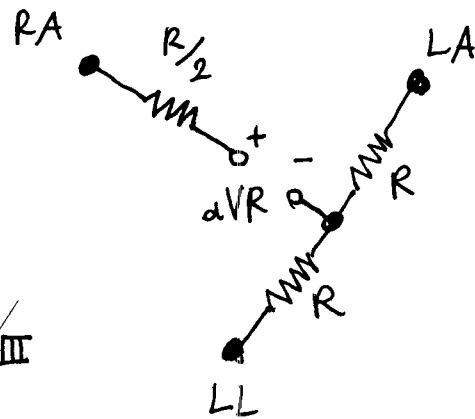


$$aVR = RA - \frac{1}{2}(LA + LL)$$

$$aVL = LA - \frac{1}{2}(RA + LL)$$

$$aVF = LL - \frac{1}{2}(RA + LA)$$

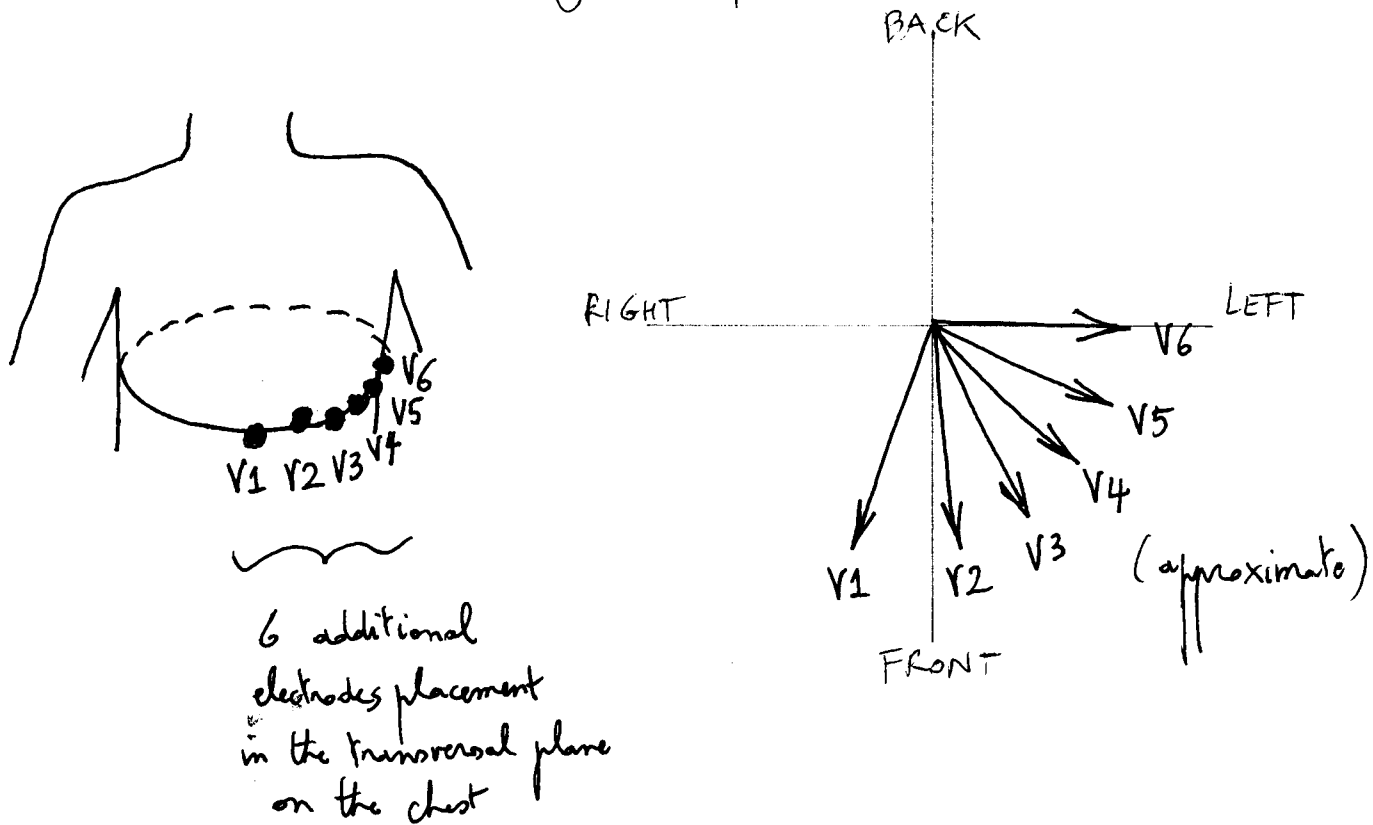
e.g.: aVR :



6 leads, and their complements, span  $360^\circ$  in  $30^\circ$  increments on a polar plot.



- Transversal plane: additional 6 leads, from additional 6 electrodes placed on the chest, in the horizontal plane perpendicular to the frontal plane.



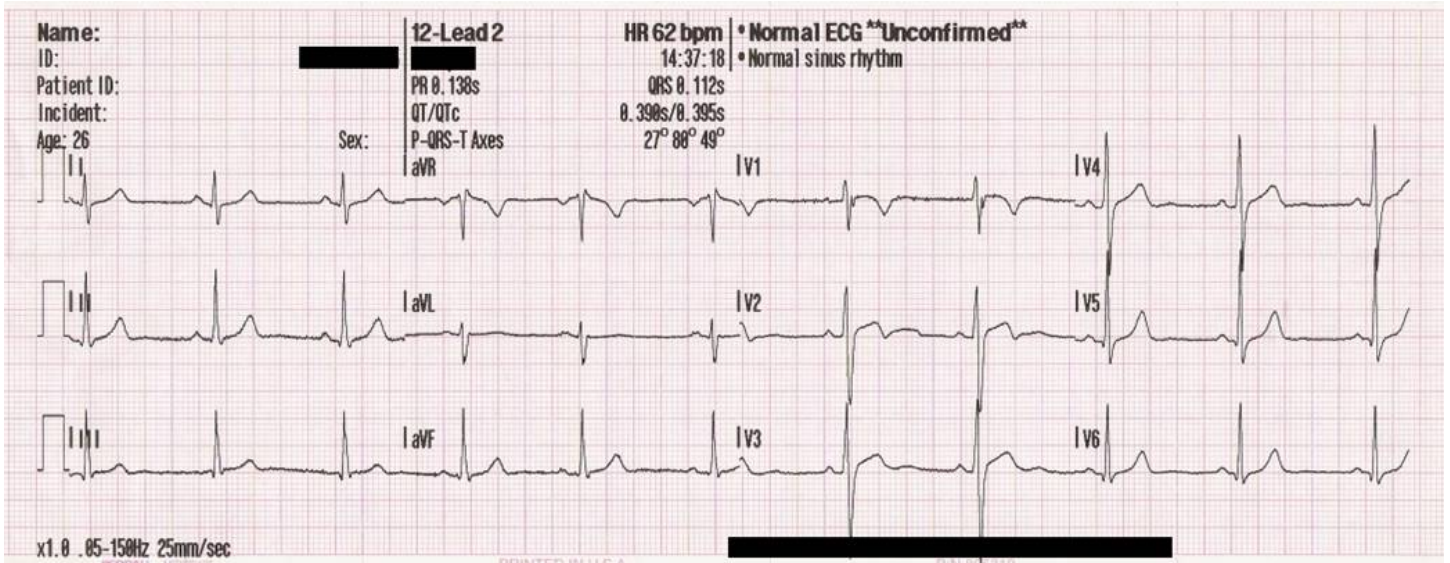
The leads V1 through V6 are taken on the 6 electrodes, relative to the Wilson Central Terminal (WCT).

- The 12-LEAD ECG combines 6 leads of the frontal plane with 6 leads of the transversal plane, from a total of 10 electrodes

- leads: I, II, III, aVR, aVL, aVF, V1, V2, V3, V4, V5, V6

- electrodes: RL (active ground reference) + RA, LA, LL, V1, ... V6

Example 12-Lead Electrocardiogram (<http://en.wikipedia.org/wiki/Electrocardiography>):



12 Leads on the Torso (ECG Learning Center, <http://ecg.utah.edu/>):

