BENG 186B: Principles of Bioinstrumentation Design

Lecture 2

Linear Circuit Analysis and Dynamical Characteristics

References

Webster, Ch. 1 (Sec. 1.9, 1.10).

The Design and Analysis of Linear Circuits, 6th Ed., Thomas, Rosa and Toussaints, Wiley 2009 (MAE 140 textbook).

http://en.wikipedia.org/wiki/Thévenin%27s theorem

Review of linear circuits

See, e.g: The Analysis and Design of Linear Circuits, 6th Ed, Thomas, Rose & Townsaints, Wiley 2009 (MAE 140 book).

- Kirchhoff's current law (KCL): conservation of dange
$$\sum I's$$
 into any node $= 0$

Currents, with sign. $I_1 \notin I_2$ Choose the direction $I_1 = 0$ of the arrows, and be

2 V's around any closed loop = 0

voltages, with sign.

Sometimes in terms of rode

Vi & Vi Vi

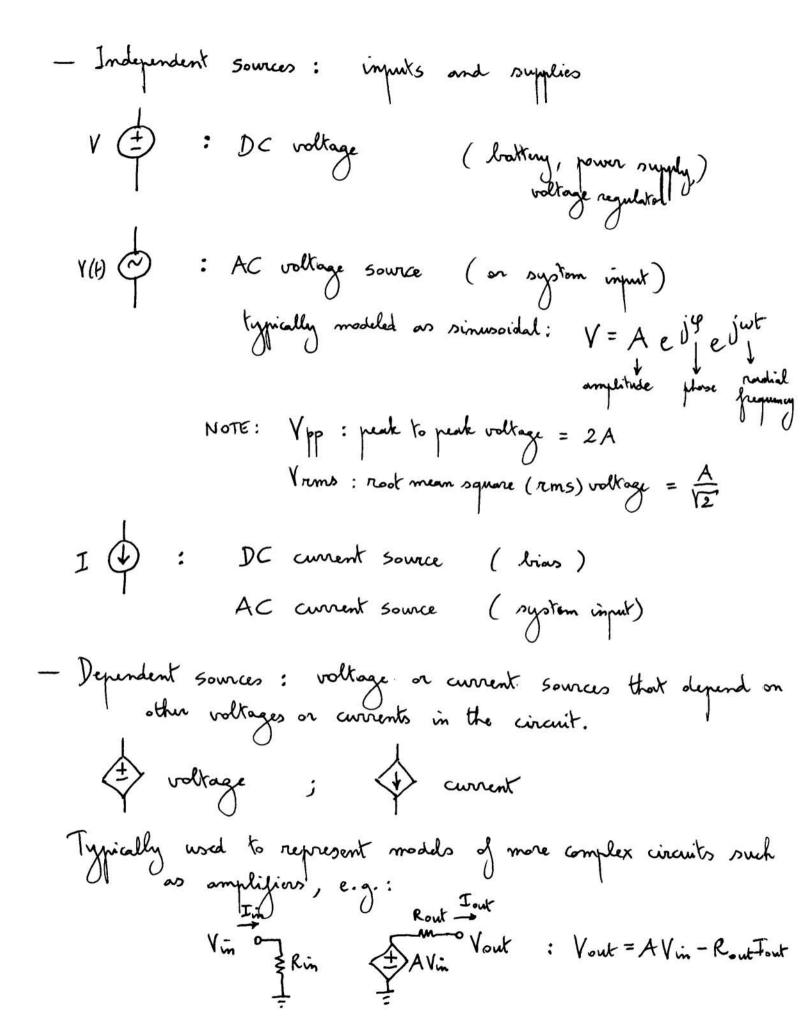
voltages: Va Wir V=Vb-Va VI 3-V3+3

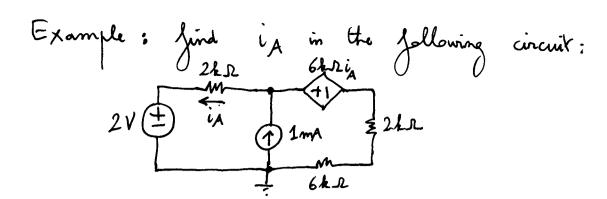
- Circuit elements: relate voltage and current (or their derivatives)

+
$$\frac{V}{R}$$
 - $\frac{V}{R}$ - $\frac{$

I = C at , ~ Z = iwc * .________ V= LatI, n Z= jwL Note: be consistent with polarities of I and V +_.... : V=-R.I

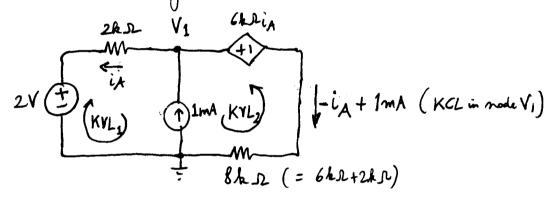
V1 + V2 - V4-V3=0





Solution:

Label all unknown voltages & currents, write out known voltages and currents (from KYL&KCL), and combine circuit elements:



$$KVL_1: V_1 = 2V + 2k\Omega. i_A$$

$$KVL_2: V_1 = 8k\Omega(-i_A + 1mA) + 6k\Omega i_A = 8V - 2k\Omega \cdot i_A$$

Note: combining circuit elements:

$$Z_1 \quad Z_2 \quad \Rightarrow \quad Z \quad Z = Z_1 + Z_2 \quad \text{series combination}$$
 $Z_1 \quad Z_2 \quad \Rightarrow \quad Z \quad Z = Z_1 + Z_2 \quad \text{parallel combination}$
 $Z_1 \quad Z_2 \quad \Rightarrow \quad Z \quad Z = \frac{1}{Z_1 + Z_2} \quad \text{or} \quad Z = \frac{1}{Z_1 + Z_2} \quad \text{parallel combination}$

· Series Combination:

$$KCL: I_1 = I_2 = I$$

$$KYL: Y = Y_1 + Y_2$$

=)
$$Z = \frac{V}{I} = \frac{Z_1.1 + Z_2.T}{I} = Z_1 + Z_2$$

=) IMPEDANCES ADD IN SERIES

· Parallel combination:

$$KCL: I = I_1 + I_2$$

= $\frac{V_1}{Z_1} + \frac{Y_2}{Z_2}$

$$KVL: V_1 = V_2 = Y$$

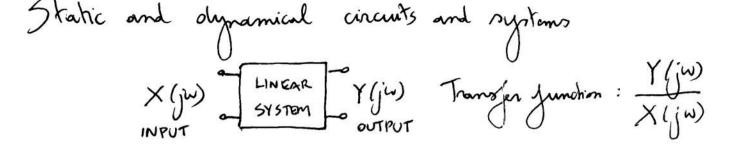
$$=) Z = \frac{V}{I} = \frac{V}{\frac{V}{Z_1} + \frac{V}{Z_2}} = \frac{1}{\frac{1}{Z_1} + \frac{1}{Z_2}} = \frac{Z_1, Z_2}{Z_1 + Z_2}$$

on
$$Y = Y_1 + Y_2$$
 ADMITTANCE reciprocal of impredence

=) ADMITTANCES ADD IN PARALLEL

· Series and parallel combinations can be recursively combined to find impedance of more complex circuits:

Example: find the impedance of the following circuit between modes A and B: A My 1007/ B 100 list 17 pf T Tipf, 3 mH/ Z=R=) resistances add in SERIES Z = jwL = inductances add in SERIES Z = 1 =) conacitances add in PARALLEL =) A | | 8 pF = \$ 60 Le // \$ 8 pt 9 8 m M => Z = \frac{100 kl. (jw8nH + 10kl. + \frac{1}{jw8pF})}{100 kl. + jw8nH + 10kl. + jw8pF} (x jw 8pf) (x jw8pF) $= 100 \text{ kg} \cdot \frac{1 + \text{jw 80 ms} - \text{w}^2 64 \text{ 10}^{-21} \text{s}^2}{1 + \text{jw 880 ms} - \text{w}^2 64 \text{ 10}^{-21} \text{s}^2}$ Z = 100 kg (leftmost branch only) for $w \rightarrow 0$ and for $w \rightarrow \infty$ Sanity check: 10002 one open circuit for w→00



- X and Y can be voltage or current, or other signal types . jw is sometimes written as $D=\frac{1}{olf}$, differential operator for use in the time domain.
- ZEROTH-ORDER INSTRUMENT (Static system):

linear system with constant transfer function: static gain (or sensitivity) independent of frequency.

Circuits with only resistors are always static: the output follows the input instantaneously.

Example: Attenuator implemented as VOLTAGE DIVIDER:

Vin P II & R2 Yout R2.

 $\frac{V_{\text{out}}(j\omega)}{V_{\text{vin}}(j\omega)} = A_{\text{v}} = \frac{R_1}{R_1 + R_2} \quad \text{where} \quad 0 \leq A_{\text{v}} \leq 1$ independent of frequency

useful where it is desirable to attenuate the amplitude (or range) of a voltage signal for jurther processing.

NOTE 1: Attenuation due to voltage division is not always intentional in the design, and may be the effect of non-ideal source and system impudances, e.g.: Vs Rs Rin SYSTEM INSTRUMENT INPUT IMPEDANCE BIOPOTENTIAL SKIN AND ELECTRODE IMPEDANCE on trady to instrument $=) \quad \forall \dot{m} = \frac{\dot{k}\dot{m}}{\dot{k}\dot{m} + \dot{k}\dot{s}}$ =) Good DESIGN: Vin ≈ Vs Ja Rin≫ Rs Signal on real measured by the -> minimize skin and the Charley electrode impedance -) maximize instrument input impedance NOTE 2: For frequency-dependent impedances nother than resistors, voltage division may implement frequency-dynaent transfer Vin P Z2 Z1 Yout $\frac{V_{\text{out}}(j\omega)}{0} = \frac{Z_1(j\omega)}{0}$ Vin (ju) ス(jw)+Z2(jw) Dynamical systems can be readily designed by clossing and implementing Z, (jw) and Z2 (jw):

- FIRST - ORDER INSTRUMENT:
$$\frac{Y(j\omega)}{X(j\omega)} = \frac{b_1 j\omega + b_0}{d_1 j\omega + d_0}$$
 (single pole)

Example: RC jirst-order lowpars filter:
$$\frac{V_{out}(j\omega)}{V_{in}(j\omega)} = \frac{1}{1+j\omega Z}$$

$$Z_{1}(j\omega) = \overline{j\omega}$$

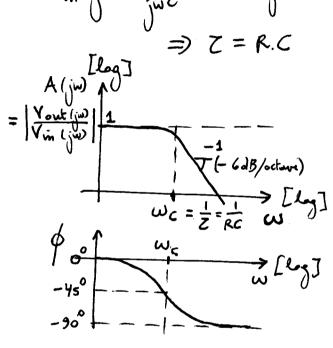
$$Z_{2}(j\omega) = R$$

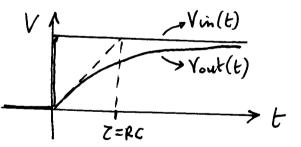
· Frequency response:

$$A(j\omega) = \frac{1}{\sqrt{1+\omega^2 z^2}}$$

· Step response:

$$V_{out}(t) = 1 - e^{-t/z}$$





More generally: linear circuits with resistive elements (R's) and with one equivalent sugramical element (Lor C), have first order dynamics.

NOTE: combine series or parallel instances of same type (Lor C) hynamical elements into single equivalent elements.

Example:
$$t=0$$

$$V_{s} \stackrel{!}{\oplus}$$

$$V_{s} \stackrel{!}{\oplus}$$

Reg = R₁+R₂

Reg = R₁+R₂

$$= V_{S} + V_{S} +$$

2 equations; eliminate V, by differentiating the second: $0 = \frac{dV_1}{dt} + \text{Reg. } \frac{dI}{dt}$

=) - Reg. Ceg.
$$\frac{dI}{dt}$$
 = I =) $I = I_0 \cdot e^{-\frac{t}{2}}$

volere Io is given by initial conditions.

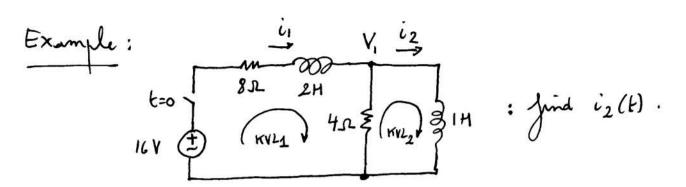
e.g. if $V_1(0) = 0$ (no initial charge on the capaciton) Hen $I_0 = V_5/R_{eq}$

- SECOND - ORDER INSTRUMENT:
$$\frac{Y(j\omega)}{X(j\omega)} = \frac{k_2(-\omega^2) + k_2}{a_2(-\omega^2) + a_2}\frac{k_2}{j\omega + a_0}$$

(two poles, possibly complex)

Example: RLC occord-order lowgons: $\frac{V_{out}(j\omega)}{V_{in}(j\omega)} = \frac{1}{1 + \frac{25j\omega}{\omega_n} - \frac{\omega^2}{\omega_n^2}}$
 $\frac{V_{out}(j\omega)}{V_{in}(j\omega)} = \frac{1}{j\omega C}$
 $\frac{V_{out}(j\omega)}{V_{in}(j\omega)} = \frac{1}{j\omega C}$

SECOND-ORDER dynamics.



Solution: use KVL, KCL to get a second-order ODE. (no sinusocidal input, so use
$$D = \frac{d}{dt}$$
 nather than $jw!$)

 $KVL_1: -16 + 8i_1 + 2\frac{di_1}{dt} + 4(i_1-i_2) = 0$ (1)

$$KVL_2: 4(i_2-i_1)+1.\frac{di_2}{dt}=0$$
 (2)

Eliminate
$$i_1: (2): i_1 = i_2 + \frac{1}{4} \frac{di_2}{dt}$$
 } substitute in (1)
$$\frac{1}{dt}(2): \frac{di_1}{dt} = \frac{di_2}{dt} + \frac{1}{4} \frac{d^2i_2}{dt^2}$$

$$=) -16 + (8i_2 + 2\frac{di_2}{dt}) + (2\frac{di_2}{dt} + \frac{1}{2}\frac{d^2i_2}{dt^2}) + \frac{di_2}{dt} = 0$$

or
$$\frac{d^2i_2}{\partial t^2} + 10 \frac{di_2}{dt} + 16 i_2 = 32$$

Linear ODE log of tricks: try a solution of the form: $i_2(t) = i_{200} + A_1 e^{\lambda_1 t} + A_2 e^{\lambda_2 t}$

STEADY STATE

SOLUTION

HOMOGENEOUS SOLUTION

• STEADY STATE;
$$\frac{d}{dt} = 0$$
 and $\frac{d^2}{dt^2} = 0$ => $16i_{2\infty} = 32$ or $i_{2\infty} = 2$

• HomoGENEOUS SOL:
$$\lambda^2 + 10\lambda + 16 = 0 = 0$$
 roots: $\lambda_1 = -2$ characteristic equation $\lambda_2 = -8$ and λ_1 , λ_2 are given by initial antitions of λ_2 and λ_2 .

- Steady state:

Often we are not interested in transients, but in the output or behavior of the circuit when it settles into STEADY STATE.

• For sinusoidal inputs: use $j\omega$ rather than $D=\frac{d}{dt}$, no need to solve ODEs!

 \rightarrow Find transfer function $\frac{Y(j\omega)}{X(j\omega)} = A(\omega) e^{j\phi(\omega)}$ GAIN PHASE (simplification)

 $X(t) = cos(\omega t) = Y(t) = A(\omega). cos(\omega t + \phi(\omega))$ in steady state

. For constant inputs (such as voltage/current supplies): same, in the limit $w \rightarrow 0$

- Power dissipation: critical for bioinstrumentation, especially implanted and wireless systems!

· Power dissipated by circuit elements:

: P = V.I

 $R: P = RI^2 = \frac{V^2}{R}$

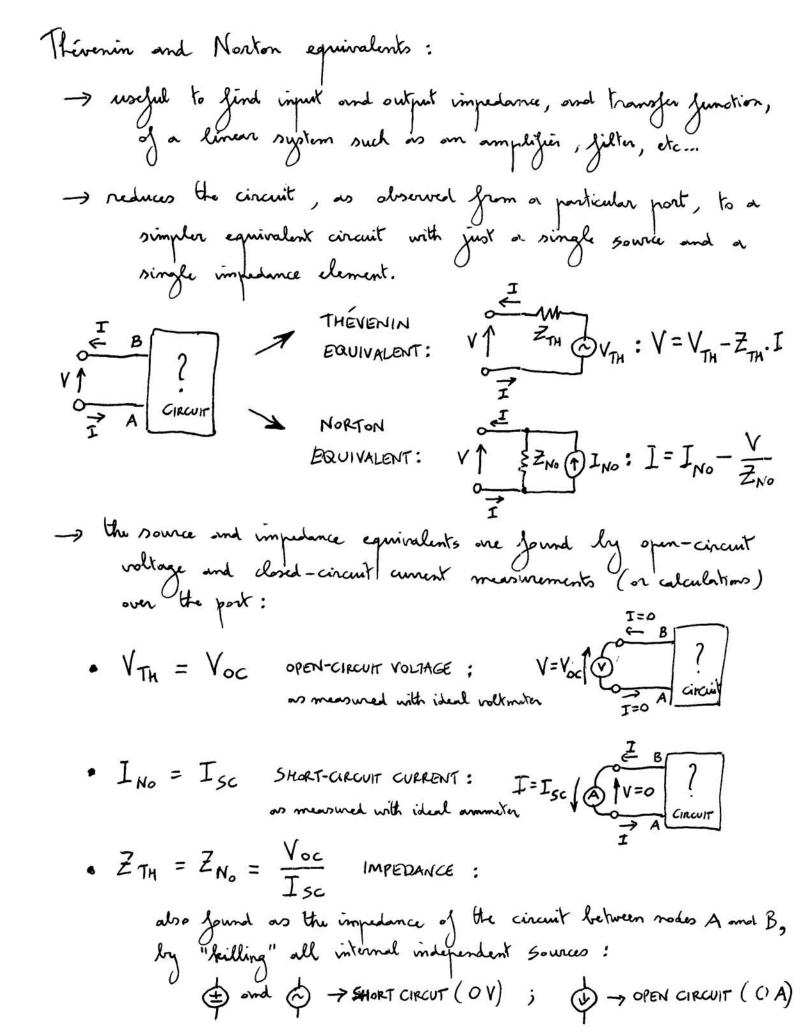
I Land C: I and V 90° out of place = ZERO AVERAGE FOWER

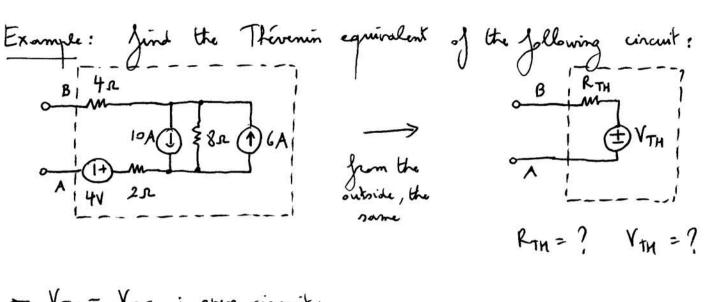
· Power supplied by independent sources: $V \stackrel{+}{=} \uparrow_{I}$ or $\stackrel{+}{\downarrow}_{V}$: P = V.INote the direction of power delivered : from lower to higher potential · Total power consumed by a circuit: METHOD 1: Sum the jower dissipated by all resistors - does not account for jower consumed by oblependent sources, e.g. amplifions in the circuit METHOD 2: Sum the power supplied by all independent sources in the circulit, e.g. the power supplies.

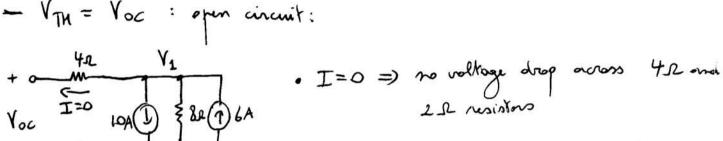
-> do not include dependent sources (e.g. amplifies) in the sum, but include their power supplies (e.g., supply drain of an amplifier) Example: 10ks KVL 5V + 0.25mA 1.25mA (1)1mA

KVL 5V + 0.25mA Los 1.25mA (1)1mA METHOD 1: Protol = PIORE + Pare = 2.51 x 0.25mA + 2.51 x 1.25mA = 3.75 mW METHOD 2: Protal = PSV + P1mA = 5V × 0.25mA + 2.5V × 1mA = 3.75mW OK! · AC power, e.g. power drawn from a biosignal source:

Average power @ ω : $P = \langle V(t), I(t) \rangle = \frac{1}{2} \text{ Real } \left(V(j\omega), I^*(j\omega) \right)$ (Steady state)







$$= \frac{10A(5)}{4V} = \frac{10A(5)}{$$

$$= V_1 - V_2 = -32V \implies V_{TH} = V_{OC} = -28V$$

$$- R_{TH} : "hill" the sources : -(1) - 3 - (5HORT)$$

$$4V \longrightarrow OA (0PEN)$$

NOTE: only independent sources should be "killed"; dependent sources remain, as they change with current or voltage.

Theorenin/Norton equivalents out input and output ports of a system give the input and output impedance and transfer Juncture of the system. -> The equivalent at the input, for an ideal load at the output, gives the input impedance. -> The equivalent at the output, for our ideal source at the input, gives the transfer function and output impedance. Vin | ER, RZ | Vout V IDEAL VOLTAGE LOAD IDLTAGE SOURCE VOLTAGE VOLTAGE = OPEN CINCUIT Voltage signal => THÉVENIN (Current => NORTON) d. INPUT No sources => You =0 (ox!)

H:
$$\begin{cases} R_{1} = \frac{R_{1}(R_{2} + \frac{1}{jwc})}{R_{1} + R_{2} + \frac{1}{jwc}} = R_{1} \cdot \frac{1 + jwR_{2}c}{1 + jw(R_{1} + R_{2})c} \\ = R_{1} \cdot \frac{1 + jwR_{2}c}{1 + jw(R_{1} + R_{2})c} \end{cases}$$

$$= R_{1} \cdot \frac{1 + jwR_{2}c}{1 + jw(R_{1} + R_{2})c}$$

Vin P = Voc R1 doesn't matter as it is driven by Vin!

Volkage dividen:
$$V_{oc} = \frac{R_2}{R_2 + \frac{1}{jwc}} \cdot V_{in} = \frac{jw R_2 C}{1 + jw R_2 C} \cdot V_{in}$$

=)
$$V_{TH} = A_V(j\omega) \cdot V_{im}$$
, where $A_V(j\omega) = \frac{j\omega R_2 C}{1+j\omega R_2 C}$

is the TRANSFER FUNCTION Vout (j')

Vin (j')

$$Z_{in}(j\omega) = R_1 \cdot \frac{1+j\omega R_2C}{1+j\omega(R_1+R_2)C}$$
 $A_{is}(j\omega) = \frac{j\omega R_2C}{1+j\omega R_2C}$ $Z_{out}(j\omega) = \frac{R_2}{1+j\omega R_2C}$

$$Z_{out}(jw) = \frac{F_2}{1 + jwF_2C}$$

Exercise: How do transfer function and output impedance change if input is CUFRENT rather than VOLTAGE?