

Modelling Transients in Action Potentials



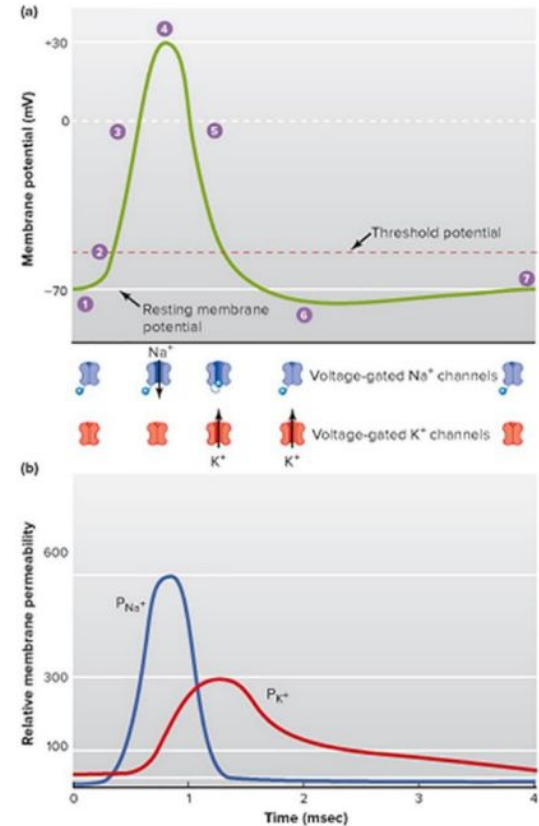
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Background ^[1,5]

- Neuron is the functional unit of nervous system
 - Afferent neuron: Information into CNS (brain & spine) from peripheral endings
 - Efferent neuron: Information out of CNS to effector cells (glands, muscles, neurons)
 - Interneurons: integrators and signal changers, only inside the CNS
- Neurons rely on chemical and electrical stimuli to relay information
 - We'll be focusing on the modelling of the chemical stimuli
- Glial cells in CNS:
 - Astrocytes: regulate composition of extracellular fluid in CNS by removing potassium ions and neurotransmitters around synapses
 - Potassium relevant for action potential propagation
- Resting membrane potential: -40 to -90 mV
 - Changes in potential due to movement of ions
- Graded potentials produced from ligand-gated ion channels and mechanically gated ion channels serve as initiating stimulus for action potential
- Voltage-gated ion channels give membrane ability to undergo action potentials

Background ^[1,5]

- Calculation of resting membrane potential using:
 - Goldman-Hodgkin-Katz (GHK) equation
 - $$E = \frac{RT}{F} \ln \frac{P_K[K^+]_o + P_{Na}[Na^+]_o + P_{Cl}[Cl^-]_i}{P_K[K^+]_i + P_{Na}[Na^+]_i + P_{Cl}[Cl^-]_o}$$
 - T=temperature, n=valence, R=gas constant, F = Faraday's constant
- Na⁺/K⁺- ATPase pump sets up concentration gradients
 - Greater flux of K⁺ out of cell than Na⁺ into cell due to greater permeability (leak channels) for K⁺
 - Negative membrane (resting potential) develops
 - Na⁺ has low permeability but large electrochemical gradient
 - Local membrane brought to threshold voltage by depolarizing stimulus
 - Current through voltage gated Na⁺ channels rapidly depolarizes membrane, causing more Na⁺ channels to open
 - Inactivation of Na⁺ channels, delayed opening of K⁺ channels halts membrane depolarization
 - Outward current through open voltage-gated K⁺ channels repolarizes membrane back to negative potential
 - Na⁺ channels go from inactivated to closed state
 - K⁺ channels close, returning membrane potential to resting value.

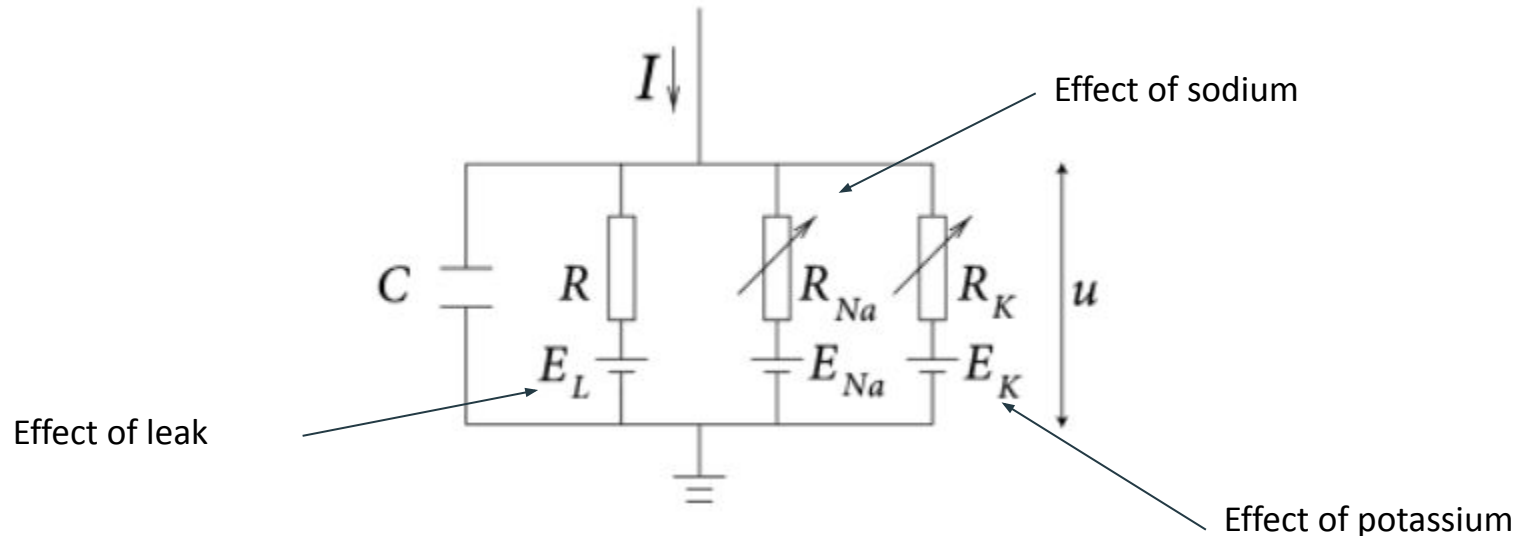


Clinical Relevance [6]

- Early epilepsy is clinical symptom of patients with CDKL5-deficiency disorder
 - Whole-cell patch-clamp recordings revealed higher action potential firing rate and lower rebase in CDD organoids, indicating increased neuronal excitability
 - Dysfunction of voltage-gated ion channels in CDD neurons that leads to hyperexcitability
 - Higher Na^+ and K^+ current densities and negative shift in Na^+ channel activation
- The above is observed in Rett syndrome patients as well
- Change in current densities and channel activation affects excitation and firing rate
 - This could be modelled in a complex system in Simulink

Hodgkin-Huxley Model^[3,4]

- Cell membranes can be modeled as a capacitor in parallel with an ionic current.
 - Hodgkin-Huxley: current is split up by charged molecules (sodium, potassium, and chlorine)
 - Model based on the propagation of an electrical signal along a squid giant axon



Hodgkin-Huxley Model (Part 2)^[3,4]

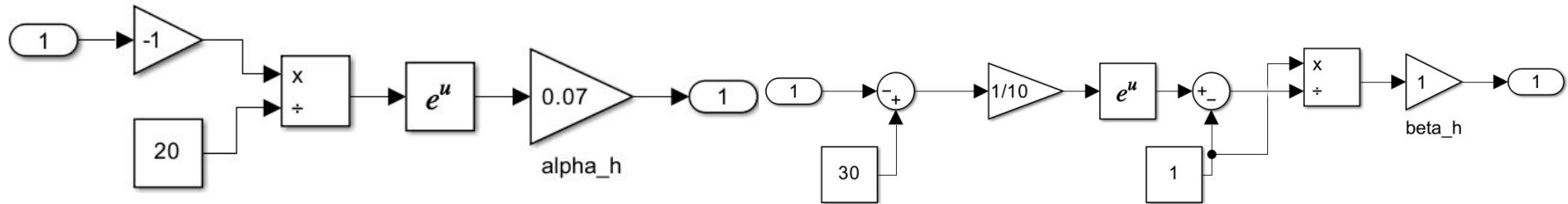
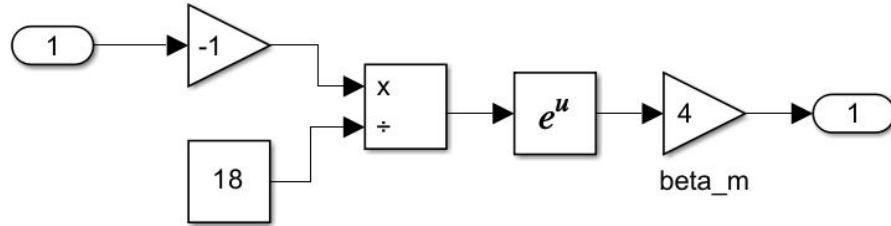
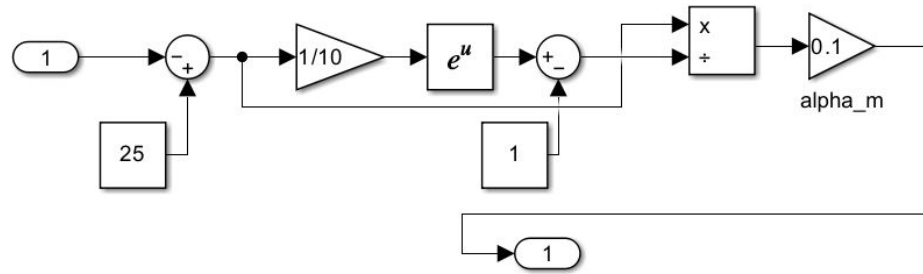
- Let m^3h represent the effects of sodium conductance, n^4 be the effects of potassium conductance.
 - α and β are numerical values depending on the voltage potential
 - g values are constants with respect to each ion

$$C_m \frac{dv}{dt} = -\bar{g}_K n^4 (v - v_K) - \bar{g}_{Na} m^3 h (v - v_{Na}) - \bar{g}_L (v - v_L)$$

$$\frac{dm}{dt} = \alpha_m (1 - m) - \beta_m m$$

$$\frac{dn}{dt} = \alpha_n (1 - n) - \beta_n n$$

$$\frac{dh}{dt} = \alpha_h (1 - h) - \beta_h h$$



$$\alpha_m = 0.1 \frac{25 - v}{\exp\left(\frac{25-v}{10}\right) - 1},$$

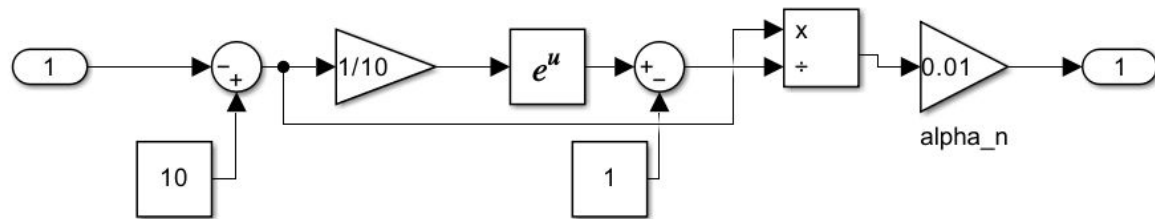
$$\beta_m = 4 \exp\left(\frac{-v}{18}\right),$$

$$\alpha_h = 0.07 \exp\left(\frac{-v}{20}\right),$$

$$\beta_h = \frac{1}{\exp\left(\frac{30-v}{10}\right) + 1},$$

$$\alpha_n = 0.01 \frac{10 - v}{\exp\left(\frac{10-v}{10}\right) - 1},$$

$$\beta_n = 0.125 \exp\left(\frac{-v}{80}\right).$$



$$\alpha_m = 0.1 \frac{25 - v}{\exp\left(\frac{25-v}{10}\right) - 1},$$

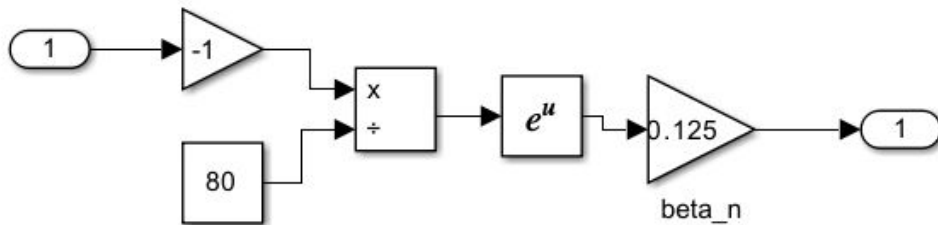
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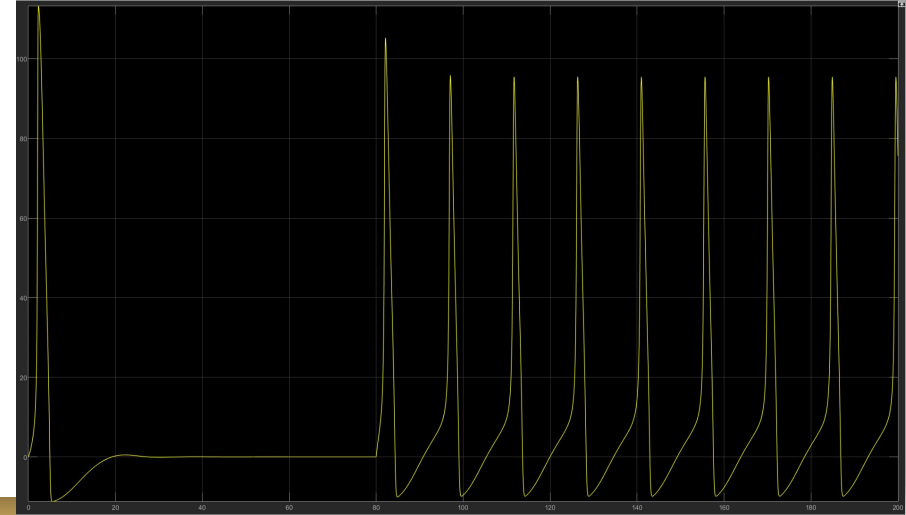
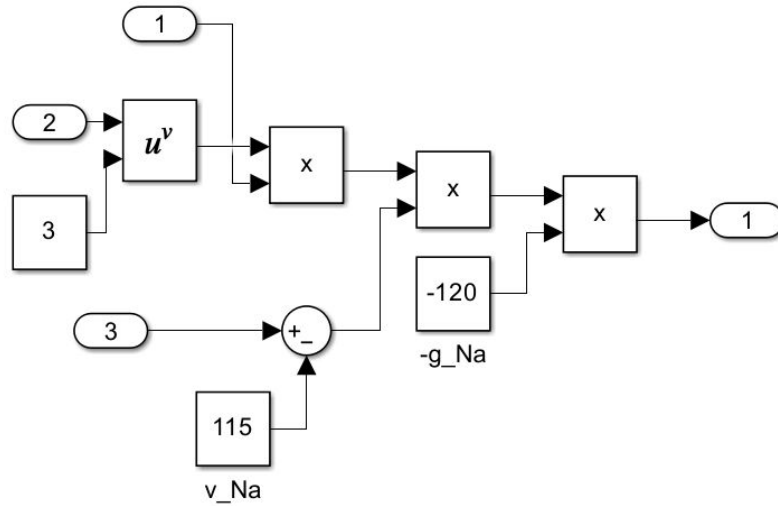
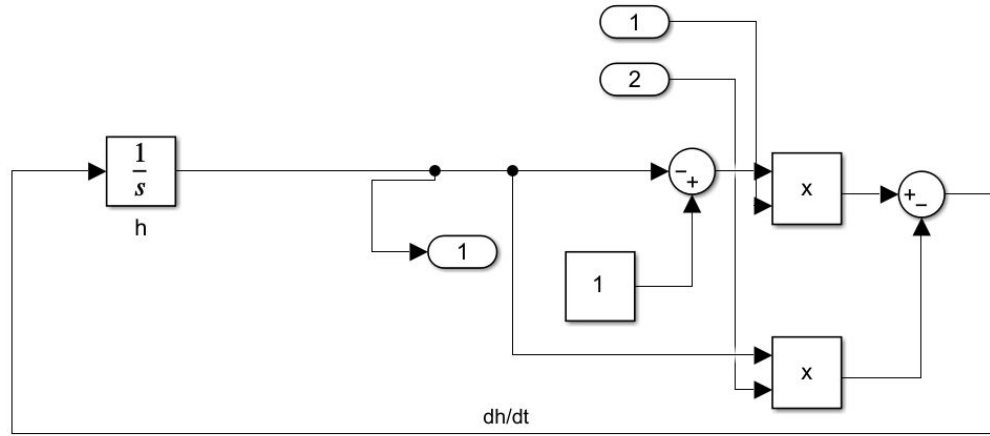
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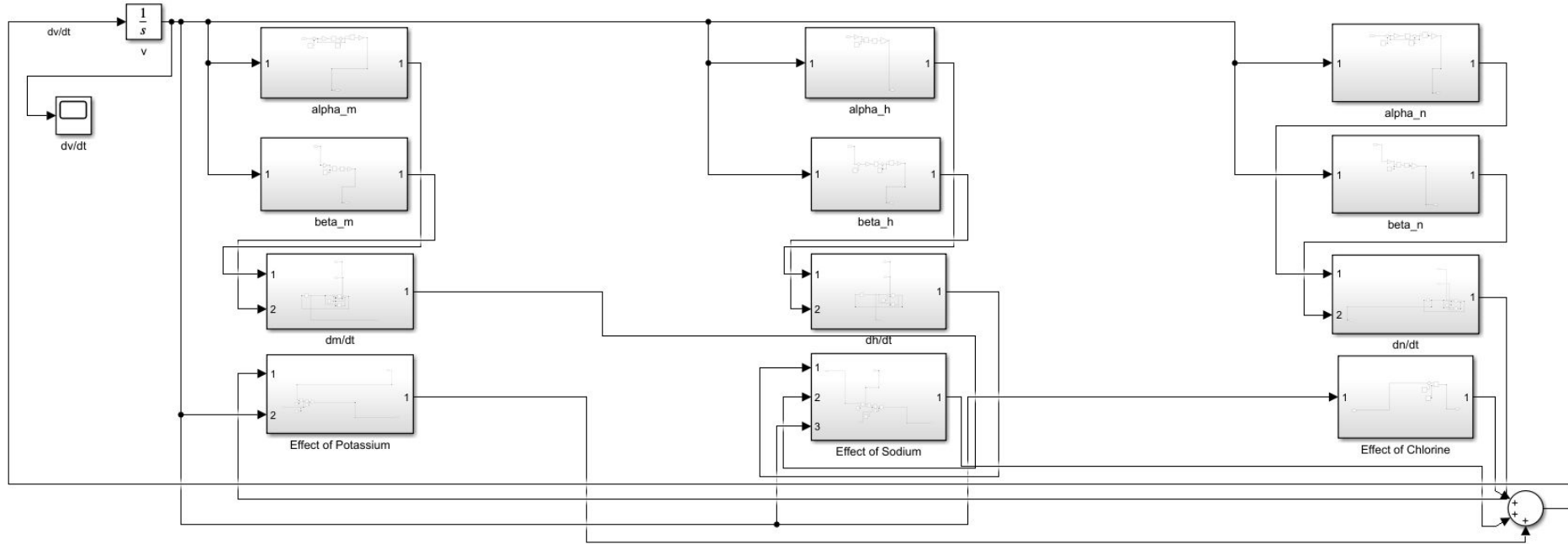
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Hodgkin-Huxley Applied



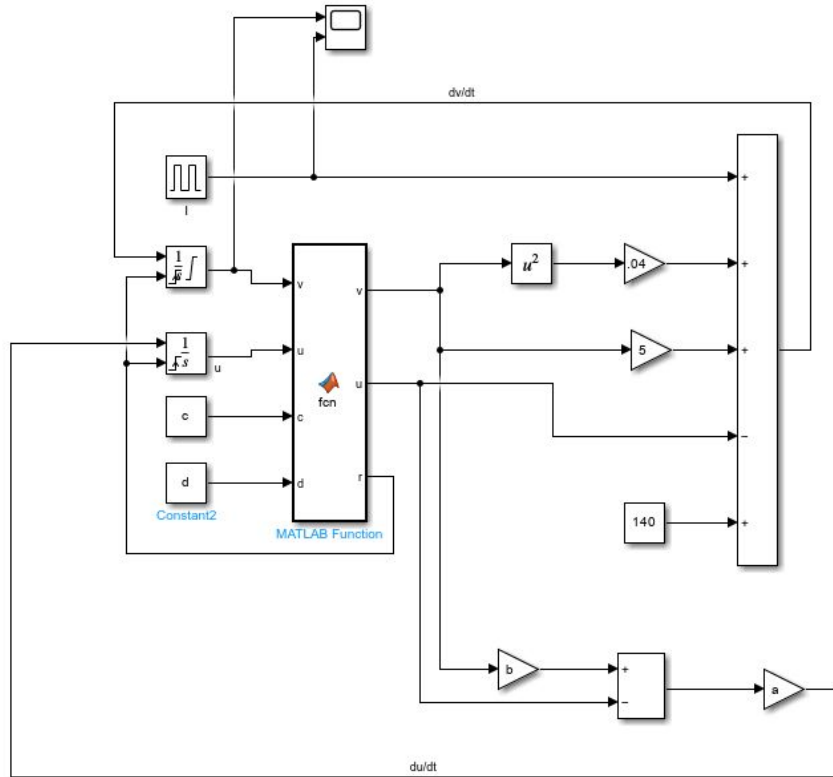
Izhikevich Model^[2]

- Designed to reproduce the spiking and bursting behavior of known types of cortical neurons.
 - Combines the biological plausibility of Hodgkin–Huxley-type dynamics and the computational efficiency of integrate-and-fire neurons.
 - Modelled using a 2D system of ODEs
- This model allows for the recreation of complex neuronal behaviour
 - Simplest canonical model of the Hodgkin Huxley class of models

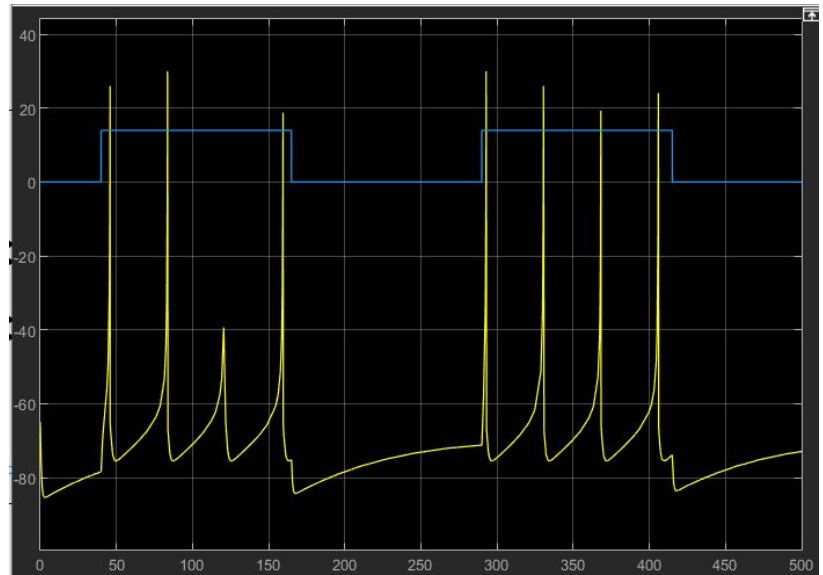
$$\begin{aligned}v' &= 0.04v^2 + 5v + 140 - u + I \\u' &= a(bv - u)\end{aligned}$$

$$\text{if } v \geq 30 \text{ mV, then } \begin{cases} v \leftarrow c \\ u \leftarrow u + d. \end{cases}$$

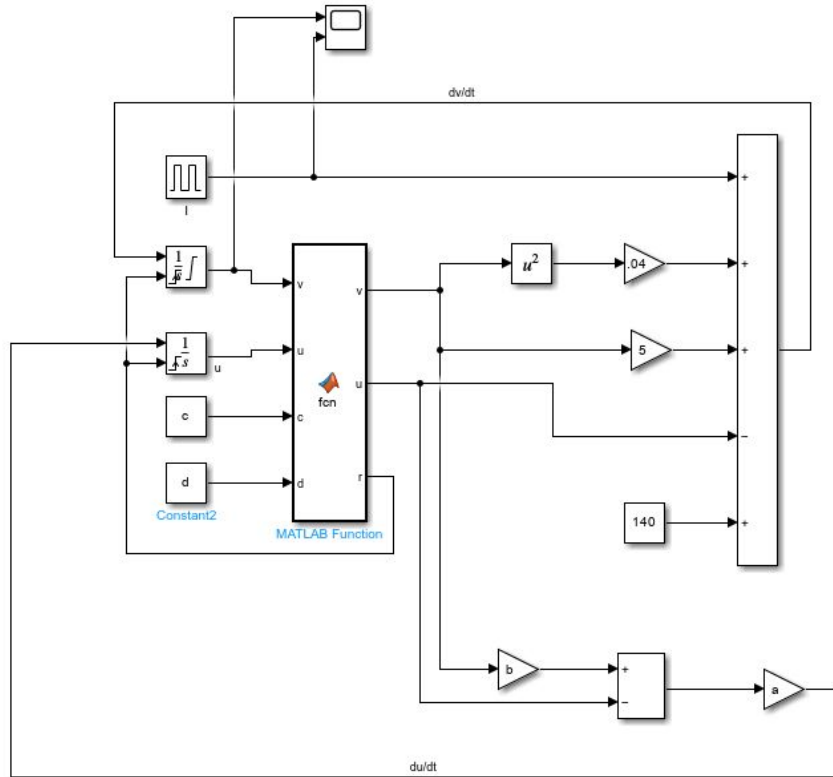
Izhikevich Model - Individual Spiking [2]



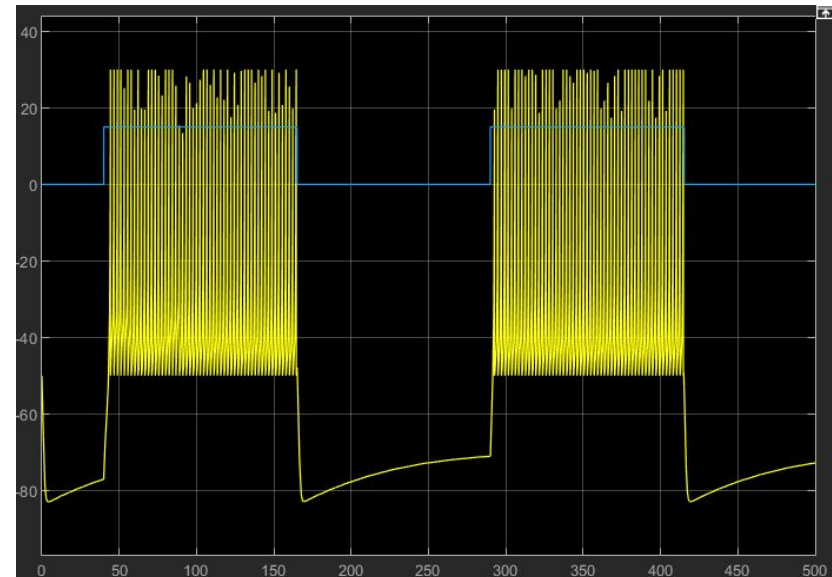
Izhikevich Model
 $dv/dt = 0.04v^2 + 5v + 140 - u + I$
 $du/dt = a(bv - u)$



Izhikevich Model - Bursting ^[2]



Izhikevich Model
 $dv/dt = 0.04v^2 + 5v + 140 - u + I$
 $du/dt = a(bv - u)$



Future Directions

- Our models simulate action potentials looking at the basic ions during “normal” physiological behavior and cell signaling
- In truth, neuronal signaling is far more complex, and includes glutamatergic signaling and GABAergic signaling
 - In graduate level neuroengineering and study, this could be modelled more in depth
 - Requires more subsystems
- As indicated by clinical relevance slide:
 - Voltage gated and ligand gated channels can be affected by genetic mutations and disorders
 - Leads to different conditions for depolarization and repolarization
 - Can play with initial conditions more
 - With biosensors or some more patient specific data, the model can be adapted
- We would want to additionally analyze perturbations in the model to identify potential treatment pipelines

Acknowledgements

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References

- [1] Cauwenberghs, G. Lecture 7 Notes: *Origins of biopotentials. Excitable Cells. Nernst and resting potentials. Action Potentials* . 2022 Jan.
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- [4] Nelson ME(2011) Electrophysiological models of neural processing. Wiley Interdisciplinary Reviews: Systems Biology and Medicine, 3: 74-92.
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