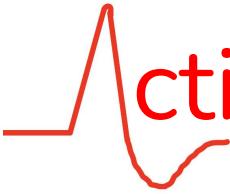


# Modelling Transients in Action Potentials



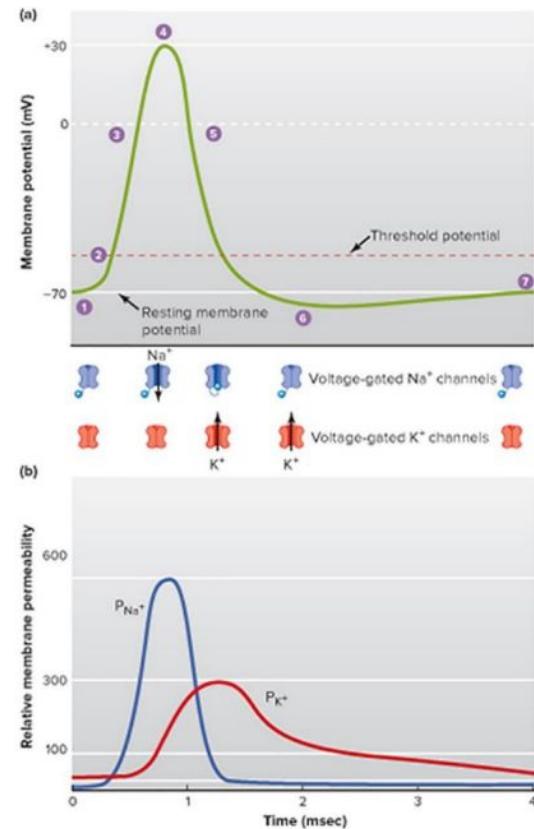
Neel Dhar, Darin Tsui, Jay Chen

# Background [1,5]

- Neuron is the functional unit of nervous system
  - Afferent neuron: Information into CNS (brain & spine) from peripheral endings
  - Efferent neuron: Information out of CNS to effector cells (glands, muscles, neurons)
  - Interneurons: integrators and signal changers, only inside the CNS
- Neurons rely on chemical and electrical stimuli to relay information
  - We'll be focusing on the modelling of the chemical stimuli
- Glial cells in CNS:
  - Astrocytes: regulate composition of extracellular fluid in CNS by removing potassium ions and neurotransmitters around synapses
    - Potassium relevant for action potential propagation
- Resting membrane potential: -40 to -90 mV
  - Changes in potential due to movement of ions
- Graded potentials produced from ligand-gated ion channels and mechanically gated ion channels serve as initiating stimulus for action potential
- Voltage-gated ion channels give membrane ability to undergo action potentials

# Background [1,5]

- Calculation of resting membrane potential using:
  - Goldman-Hodgkin-Katz (GHK) equation
    - $$E = \frac{RT}{F} \ln \frac{P_K[K_o^+] + P_{Na}[Na_o^+] + P_{Cl}[Cl_o^-]}{P_K[K_i^+] + P_{Na}[Na_i^+] + P_{Cl}[Cl_i^-]}$$
    - T=temperature, n=valence, R=gas constant, F = Faraday's constant
- $\text{Na}^+/\text{K}^+$ - ATPase pump sets up concentration gradients
  - Greater flux of  $\text{K}^+$  out of cell than  $\text{Na}^+$  into cell due to greater permeability (leak channels) for  $\text{K}^+$ 
    - Negative membrane (resting potential) develops
    - $\text{Na}^+$  has low permeability but large electrochemical gradient
  - Local membrane brought to threshold voltage by depolarizing stimulus
  - Current through voltage gated  $\text{Na}^+$  channels rapidly depolarizes membrane, causing more  $\text{Na}^+$  channels to open
  - Inactivation of  $\text{Na}^+$  channels, delayed opening of  $\text{K}^+$  channels halts membrane depolarization
  - Outward current through open voltage-gated  $\text{K}^+$  channels repolarizes membrane back to negative potential
  - $\text{Na}^+$  channels go from inactivated to closed state
  - $\text{K}^+$  channels close, returning membrane potential to resting value.

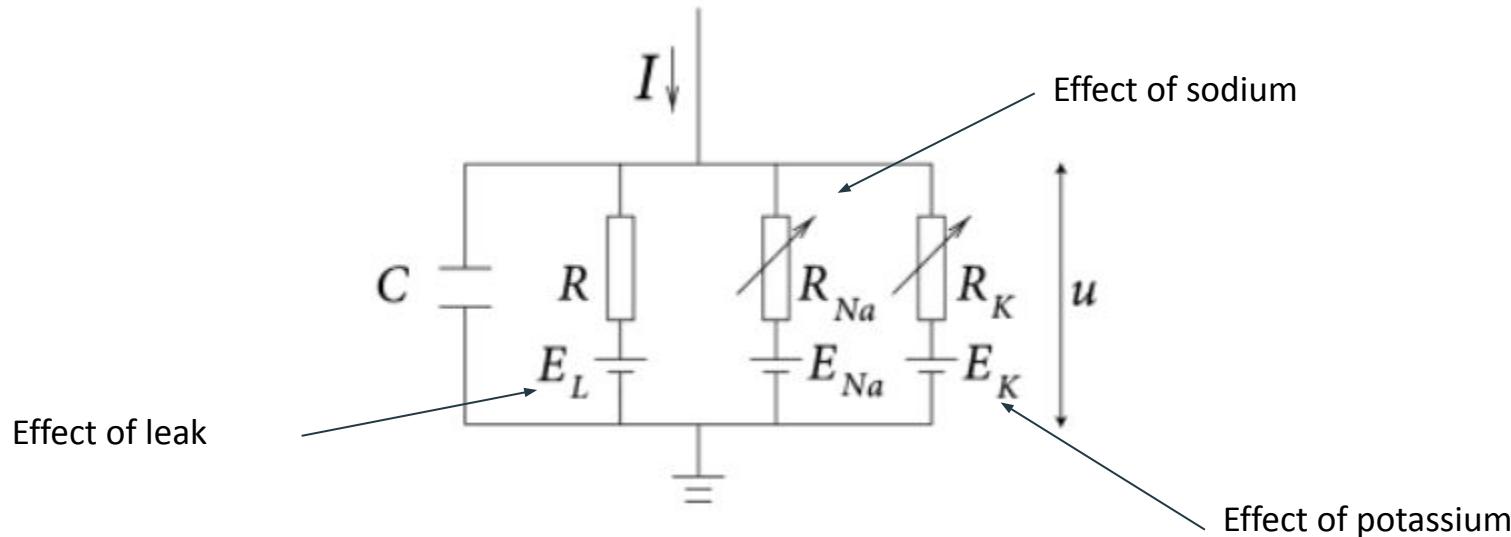


# Clinical Relevance [6]

- Early epilepsy is clinical symptom of patients with CDKL5-deficiency disorder
  - Whole-cell patch-clamp recordings revealed higher action potential firing rate and lower rehobase in CDD organoids, indicating increased neuronal excitability
  - Dysfunction of voltage-gated ion channels in CDD neurons that leads to hyperexcitability
  - Higher  $\text{Na}^+$  and  $\text{K}^+$  current densities and negative shift in  $\text{Na}^+$  channel activation
- The above is observed in Rett syndrome patients as well
- Change in current densities and channel activation affects excitation and firing rate
  - This could be modelled in a complex system in Simulink

# Hodgkin-Huxley Model<sup>[3,4]</sup>

- Cell membranes can be modeled as a capacitor in parallel with an ionic current.
  - Hodgkin-Huxley: current is split up by charged molecules (sodium, potassium, and chlorine)
  - Model based on the propagation of an electrical signal along a squid giant axon



# Hodgkin-Huxley Model (Part 2)<sup>[3,4]</sup>

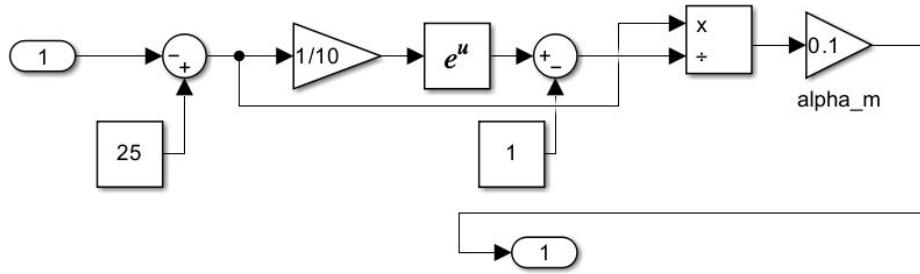
- Let  $m^3h$  represent the effects of sodium conductance,  $n^4$  be the effects of potassium conductance.
  - $\alpha$  and  $\beta$  are numerical values depending on the voltage potential
  - $g$  values are constants with respect to each ion

$$C_m \frac{dv}{dt} = -\bar{g}_K n^4 (v - v_K) - \bar{g}_{Na} m^3 h (v - v_{Na}) - \bar{g}_L (v - v_L)$$

$$\frac{dm}{dt} = \alpha_m (1 - m) - \beta_m m$$

$$\frac{dn}{dt} = \alpha_n (1 - n) - \beta_n n$$

$$\frac{dh}{dt} = \alpha_h (1 - h) - \beta_h h$$



$$\alpha_m = 0.1 \frac{25 - \nu}{\exp\left(\frac{25-\nu}{10}\right) - 1},$$

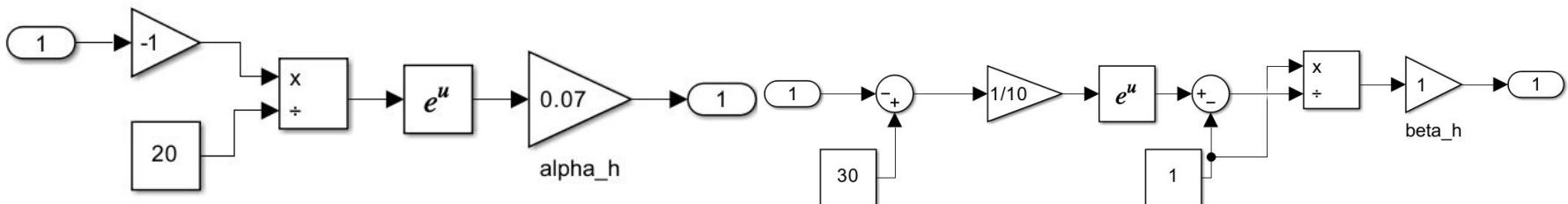
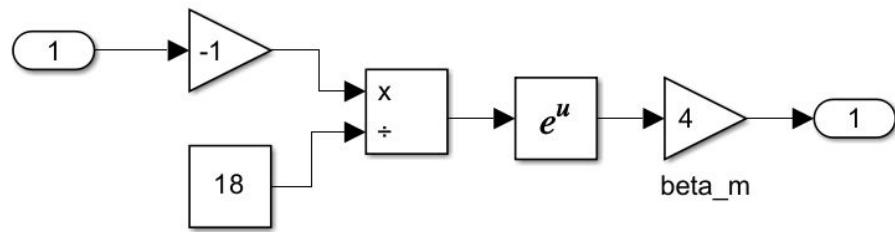
$$\beta_m = 4 \exp\left(\frac{-\nu}{18}\right),$$

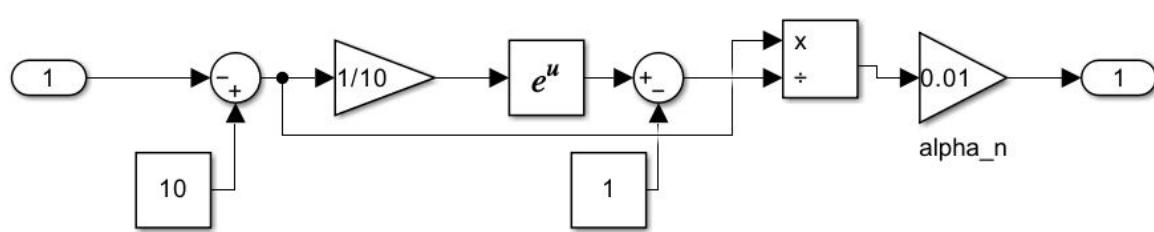
$$\alpha_h = 0.07 \exp\left(\frac{-\nu}{20}\right),$$

$$\beta_h = \frac{1}{\exp\left(\frac{30-\nu}{10}\right) + 1},$$

$$\alpha_n = 0.01 \frac{10 - \nu}{\exp\left(\frac{10-\nu}{10}\right) - 1},$$

$$\beta_n = 0.125 \exp\left(\frac{-\nu}{80}\right).$$





$$\alpha_m = 0.1 \frac{25 - \nu}{\exp\left(\frac{25-\nu}{10}\right) - 1},$$

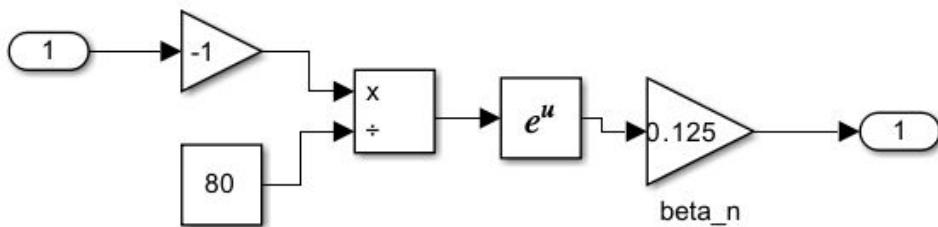
$$\beta_m = 4 \exp\left(\frac{-\nu}{18}\right),$$

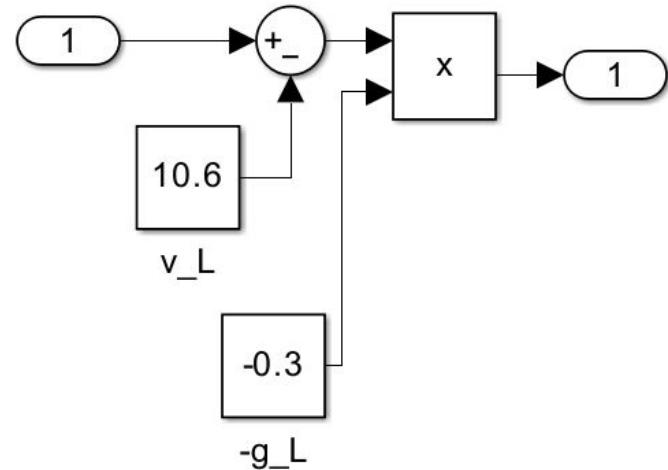
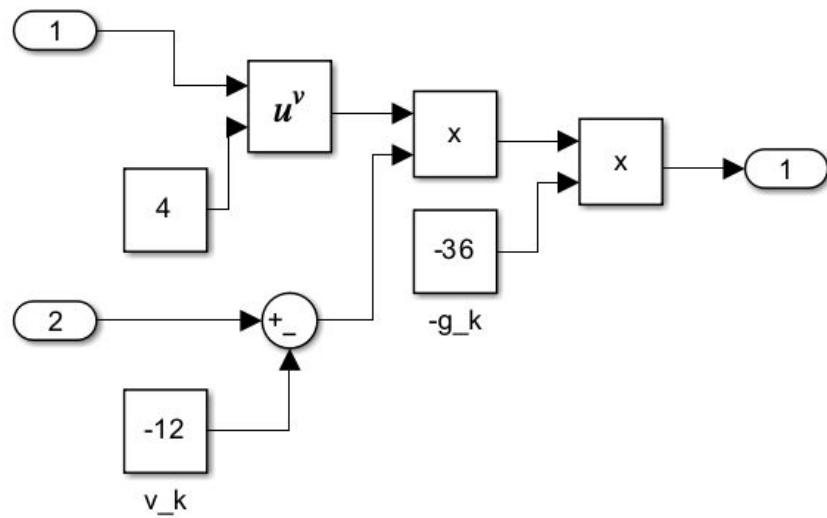
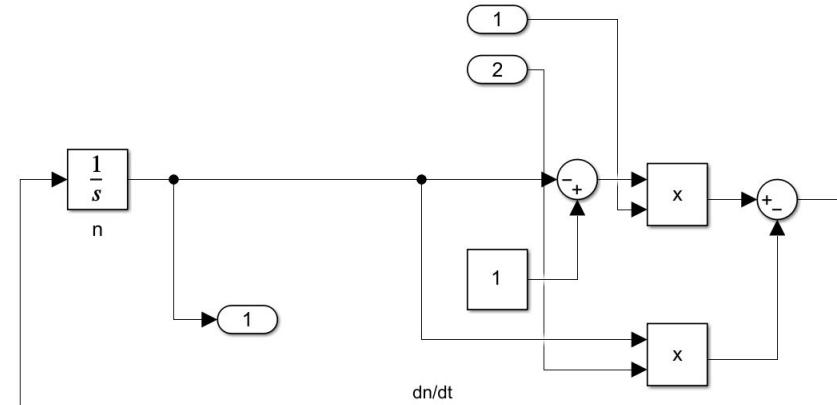
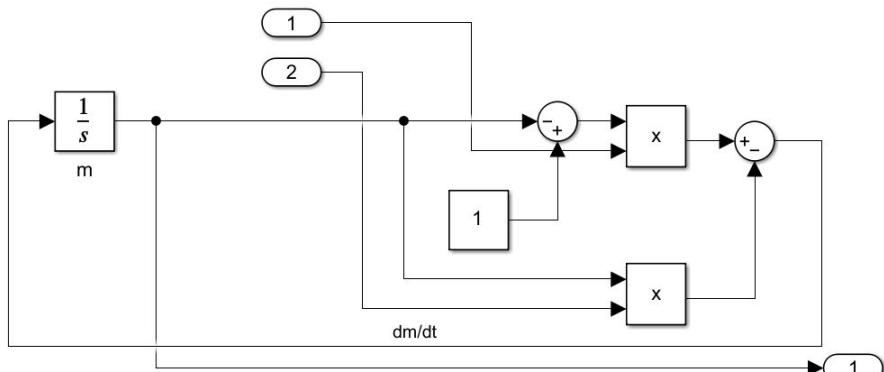
$$\alpha_h = 0.07 \exp\left(\frac{-\nu}{20}\right),$$

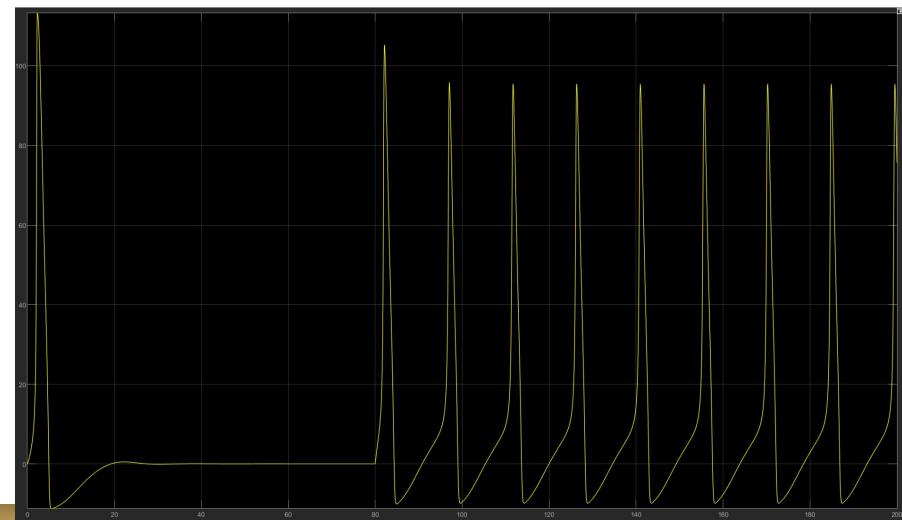
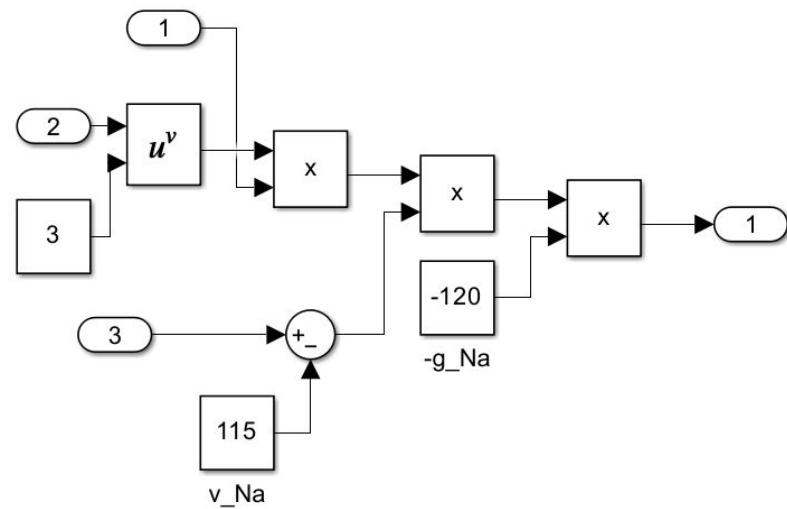
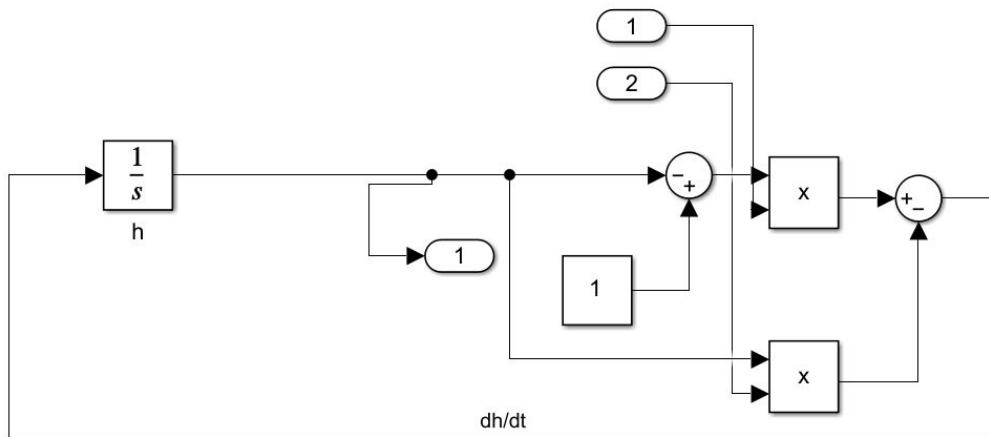
$$\beta_h = \frac{1}{\exp\left(\frac{30-\nu}{10}\right) + 1},$$

$$\alpha_n = 0.01 \frac{10 - \nu}{\exp\left(\frac{10-\nu}{10}\right) - 1},$$

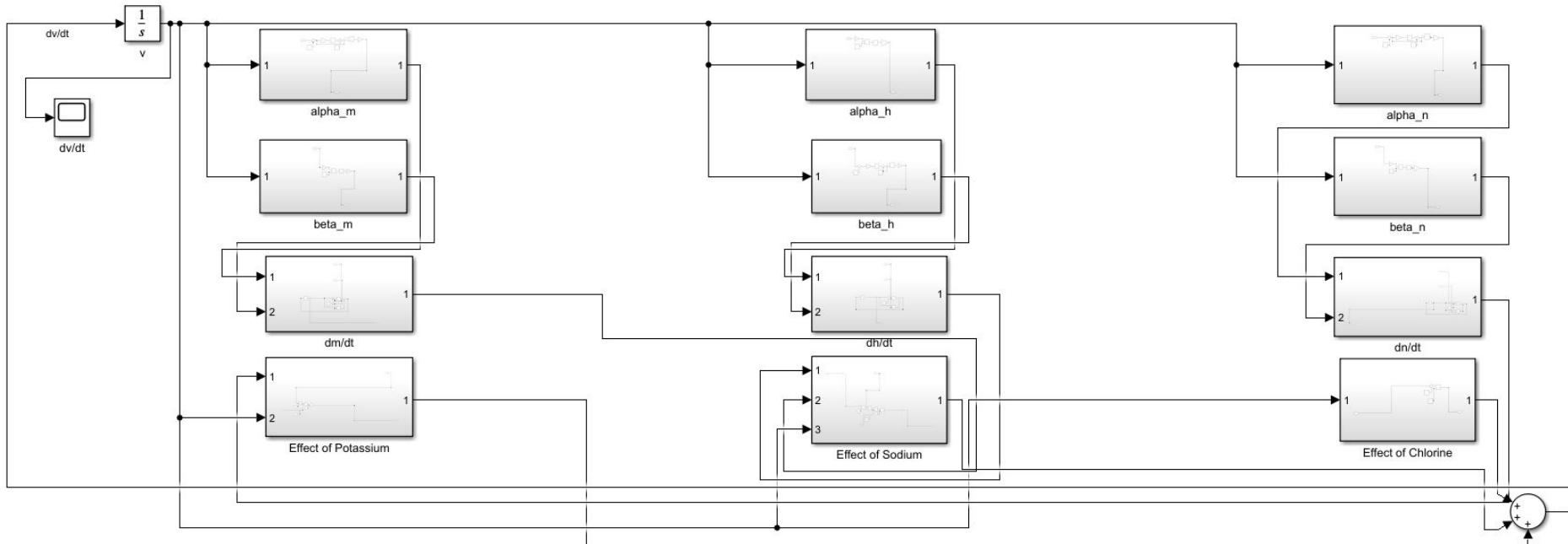
$$\beta_n = 0.125 \exp\left(\frac{-\nu}{80}\right).$$







# Hodgkin-Huxley Applied

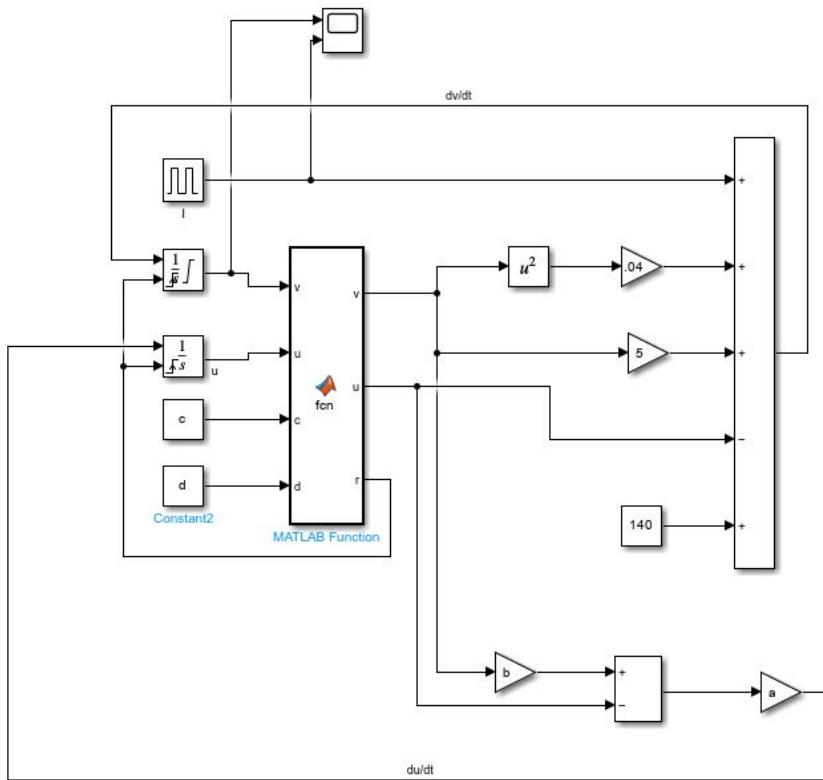


# Izhikevich Model[2]

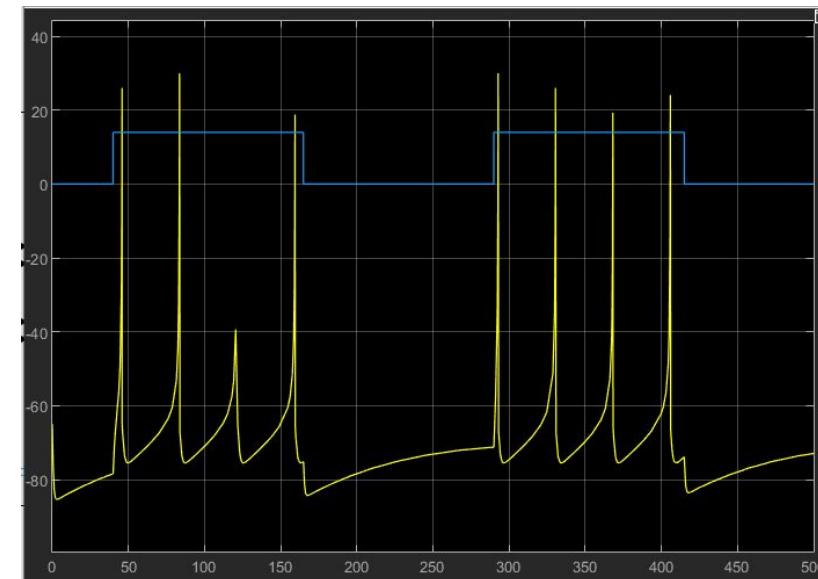
- Designed to reproduce the spiking and bursting behavior of known types of cortical neurons.
  - Combines the biologically plausibility of Hodgkin–Huxley-type dynamics and the computational efficiency of integrate-and-fire neurons.
  - Modelled using a 2D system of ODEs
- This model allows for the recreation of complex neuronal behaviour
  - Simplest canonical model of the Hodgkin Huxley class of models

$$\begin{aligned}v' &= 0.04v^2 + 5v + 140 - u + I && \text{if } v \geq 30 \text{ mV, then } \begin{cases} v \leftarrow c \\ u \leftarrow u + d. \end{cases} \\u' &= a(bv - u)\end{aligned}$$

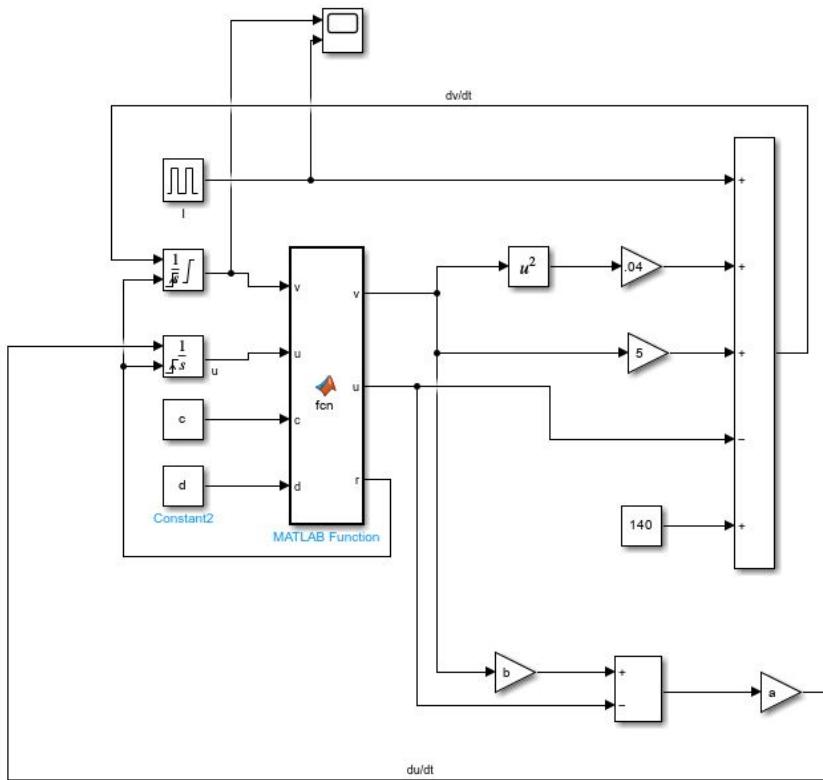
# Izhikevich Model - Individual Spiking [2]



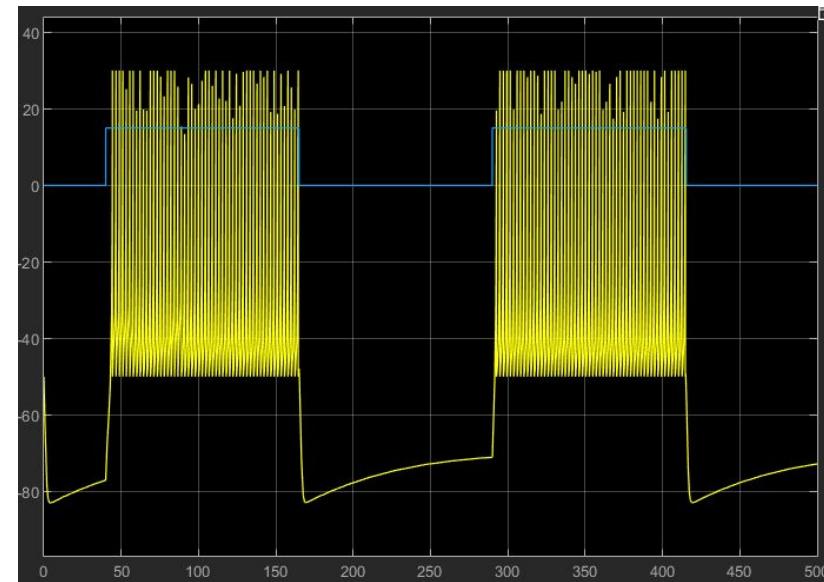
Izhikevich Model  
 $dv/dt = 0.04v^2 + 5v + 140 - y - u$   
 $du/dt = a(bv - u)$



# Izhikevich Model - Bursting [2]



Izhikevich Model  
 $dv/dt = 0.04v^2 + 5v + 140 - y - I$   
 $du/dt = a(bv - u)$



# Future Directions

- Our models simulate action potentials looking at the basic ions during “normal” physiological behavior and cell signaling
- In truth, neuronal signaling is far more complex, and includes glutamatergic signaling and GABAergic signaling
  - In graduate level neuroengineering and study, this could be modelled more in depth
  - Requires more subsystems
- As indicated by clinical relevance slide:
  - Voltage gated and ligand gated channels can be affected by genetic mutations and disorders
  - Leads to different conditions for depolarization and repolarization
  - Can play with initial conditions more
  - With biosensors or some more patient specific data, the model can be adapted
- We would want to additionally analyze perturbations in the model to identify potential treatment pipelines

# Acknowledgements

- We would like to thank Dr. Cauwenberghs for his guidance and lectures throughout the quarter



# References

- [1] Cauwenberghs, G. Lecture 7 Notes: *Origins of biopotentials. Excitable Cells. Nernst and resting potentials. Action Potentials* . 2022 Jan.
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- [4] Nelson ME(2011) Electrophysiological models of neural processing. *Wiley Interdisciplinary Reviews: Systems Biology and Medicine*, 3: 74-92.
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