

Coupled PPG-ECG Blood Pressure Monitoring Device for Hypertension Detection



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Introduction

Around 48% of all individuals in the US suffer from high blood pressure – called hypertension. Hypertension can lead to stroke, heart failure, kidney problems, among various other diseases.

Currently, the arm cuff device (sphygmomanometer) that measures blood pressure has numerous drawbacks: periodic inflation, inability to capture rapid changes, arm soreness, and inability to keep it on all the time as a monitoring device

We want to design a biomedical wristband that can accurately and continuously measure blood pressure for at-risk inpatients of hypertension-related ailments.

Our design incorporates three parts – a PPG sensor, an ECG sensor, and an XOR gate leading to a microcontroller with display.

Background & Motivation

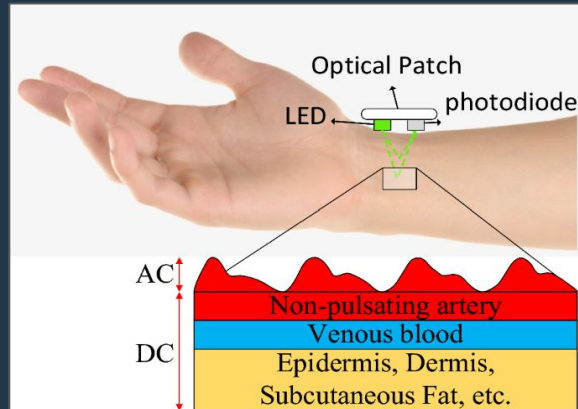
- About 46% of the adults with hypertension are not aware that they suffer from it
- Over 12.8% of all annual deaths are due to hypertension
- About 45% of adults with uncontrolled hypertension have abnormal blood pressure
- By 2025, approximately 1.56 billion adults will have hypertension



Coupled Technology Overview

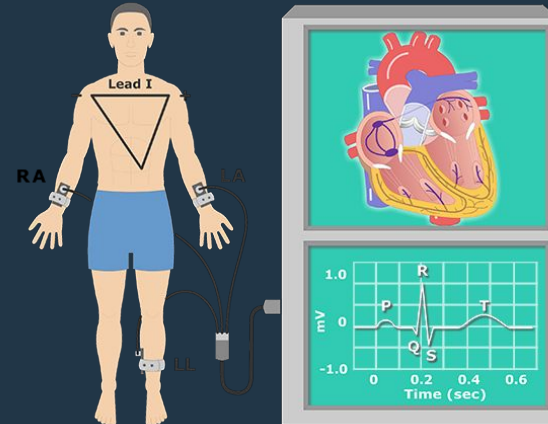
Photoplethysmography (PPG)

- Non-invasive
- Uses reflected light rays to detect blood volume change in vessels
- Gives systolic and diastolic peaks
 - Systolic peak corresponds to maximum peripheral blood volume during contraction



Electrocardiogram (ECG)

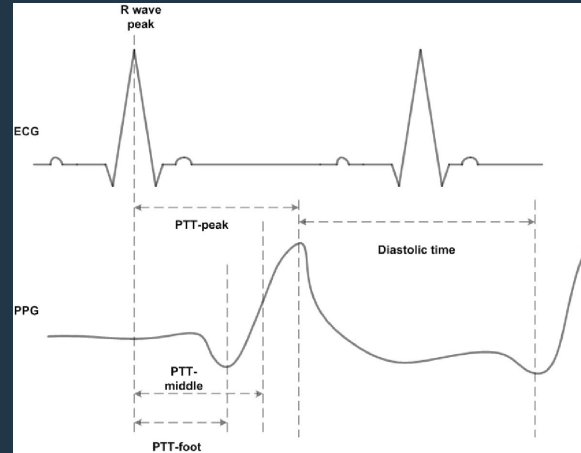
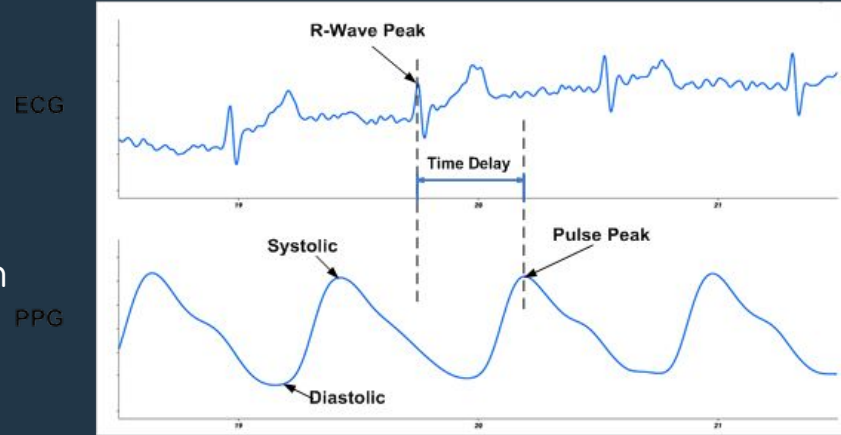
- Non-invasive
- Uses electrodes & leads to monitor heart activity
- Composed of PQRST waves representing a heartbeat's various phases
 - Focus: R-wave peak (ventricular depolarization)



Pulse Transit Time (PTT)

- PTT is the time that it takes for a pulse to travel between two points (proximal and distal points)
- Physiological Basis:
 - R wave - when blood is pumped from the heart to periphery
 - PPG Systolic peak
 - Inverse relationship between PTT and arterial wall stiffness
 - Higher BP → stiffer walls → faster pulse wave → lower PTT
- PTT can be calculated as the difference between an ECG R wave and the PPG systolic peak

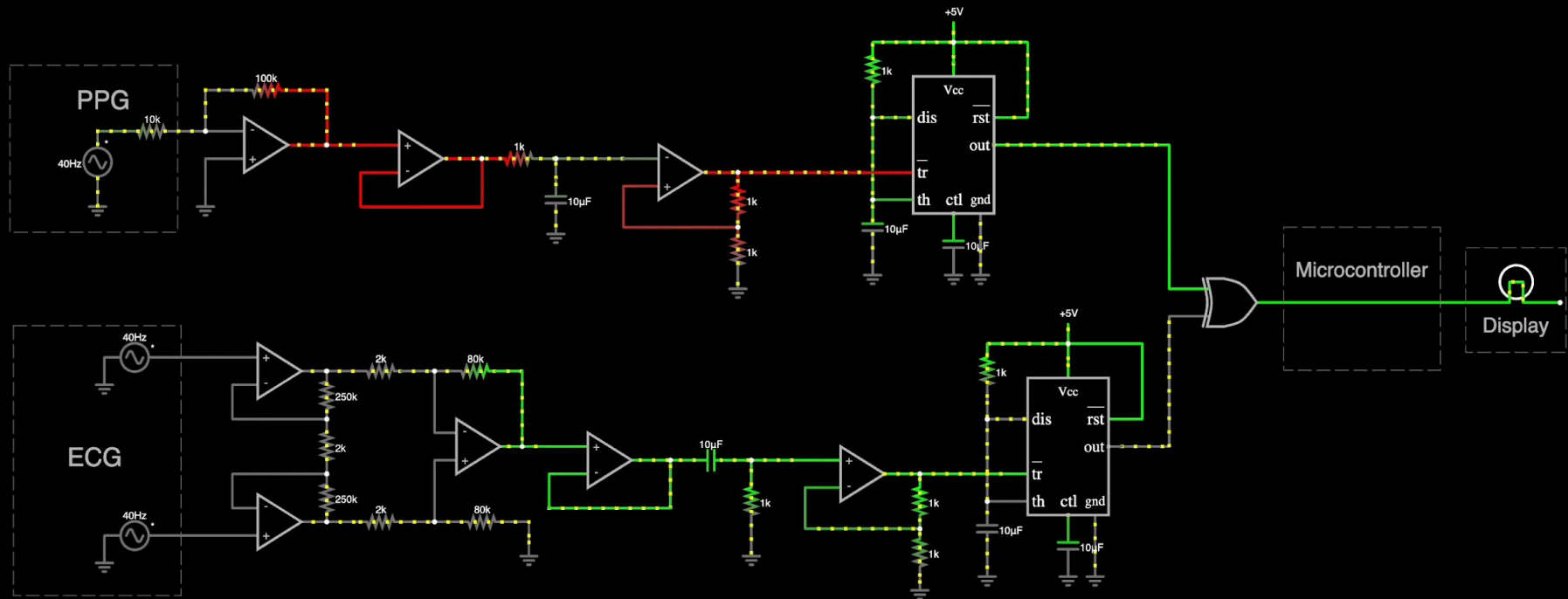
$$BP = \frac{\Delta BP}{0.7} = \frac{1}{0.7} \left(\frac{1}{2} \rho \frac{d^2}{PTT^2} + \rho gh \right)$$



Assumptions

- Circuit resistances have 0% tolerances
- Assuming a simplified hypertensive patient case
 - Systolic blood pressure between 140-190 mmHg
 - Diastolic blood pressure above 90 mmHg
- Blood pressure at the wrist fully represents the body
- Heart rate frequency is from 1-1.67 Hz → picked cutoff frequency of Low pass filter in part 1 to 5 Hz
- Uniform wave frequency
- ECG output signal 0.5-5mV
- Threshold PTT: <80ms for hypertensive people
- Assume both 555 timers will turn off at the same time
- Max time difference between ECG and PPG peaks is 110ms.
- Difference between the RR wave peak is 600ms
- Difference between Systolic wave peaks is 350ms
- All values are taken from average hypertension patient

Circuit Schematic

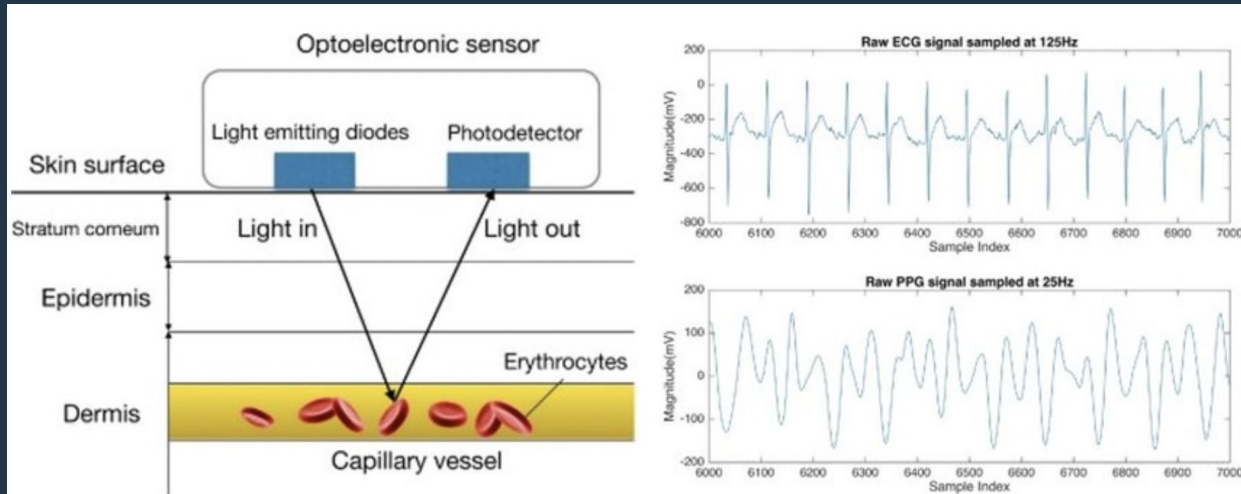


Part I Analysis



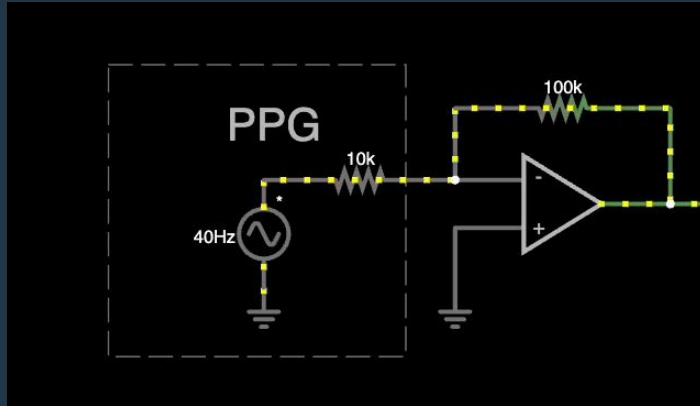
PPG sensor

- Max time difference between ECG and PPG peaks is 110ms.



Inverting Amplifier

- Used to amplify the input PPG signal while inverting it
- Inversion needed in order for the monostable 555 timer to be triggered
 - Trigger input for 555 timer: active low → input has to be below certain threshold($\frac{1}{3} V_{cc}$) to activate it



$$A = \frac{v_o}{v_s} = -\frac{R_{FB}}{R_s}$$

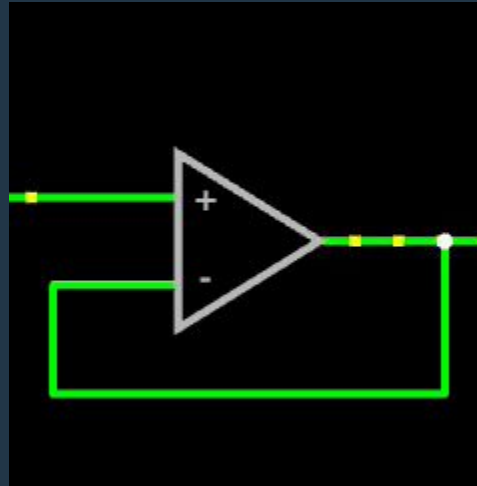
$$R_{FB} = 100k\Omega$$

$$R_s = 100k\Omega$$

$$\text{Gain} = -10$$

Buffer #1

- Isolates the previous and the next stages of the circuit so that they do not affect each other.



Passive RC low pass filter

Considerations: f_c is chosen based on frequencies of PPG sensor properties. R_1 and C_1 are calculated from that.

- Low pass filter used since PPG waves are low frequencies ~ 1-1.67 Hz
 - PPG waves can be contaminated with high frequency electronic signals, light waves, along with making systolic peaks easier to see

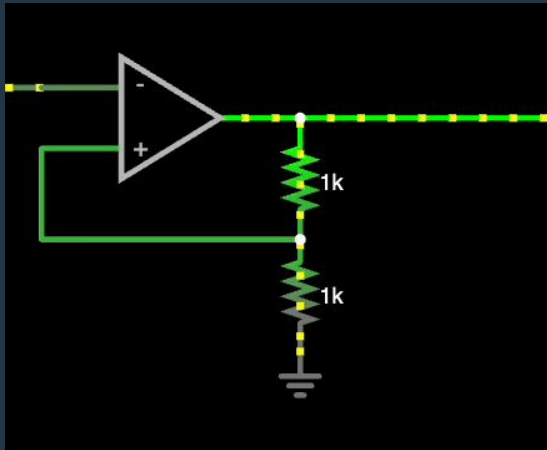


$$f_{\text{cutoff}} = \frac{1}{2\pi RC}$$

- $R_1 = 3.3 \text{ k}\Omega$
- $C_1 = 10\mu\text{F}$
- Cutoff frequency $f_c = 5\text{Hz}$

Comparator #1

- Compare the incoming voltage with the reference voltage.
- If $V_{in} < V_{ref}$, $V_{out} = V_{+}$;
- If $V_{in} > V_{ref}$, $V_{out} = V_{-}$, $V_{ref} = 2.5V$
- $V_{+} = 5V$, $V_{-} = GND$,

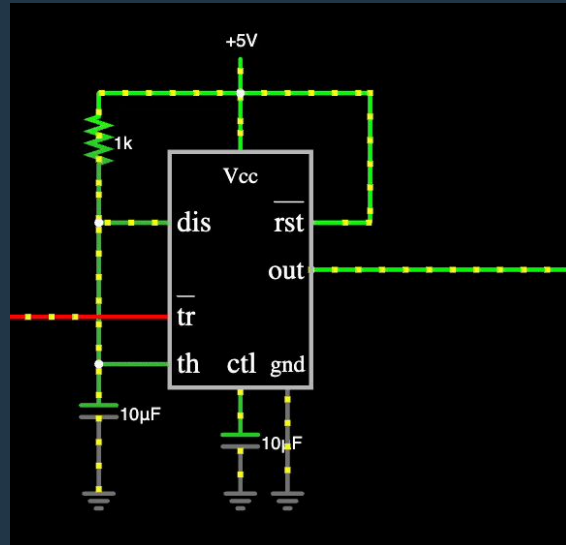


$$R_{\text{reference, ground}} = 1k\Omega$$

$$R_{\text{reference, out}} = 1k\Omega$$

555 Monostable Timer #1 (PPG)

- Threshold: Normal PPG thresholds: 0.5-5 Hz, -4~4V
- When PPG signals from previous parts exceed the threshold, timer #1 is active, output remains high for $T = RC\ln(3)$
- Time interval we want based on PPG properties: 350ms
- One set of values that might be possible: : $R = 455 \text{ kohm}$ $C = 1\mu\text{F}$



Part II Overview: ECG Sensor

Overall Goal: Measure pulse transit time (PTT) by comparing R wave and the captured pulse wave.

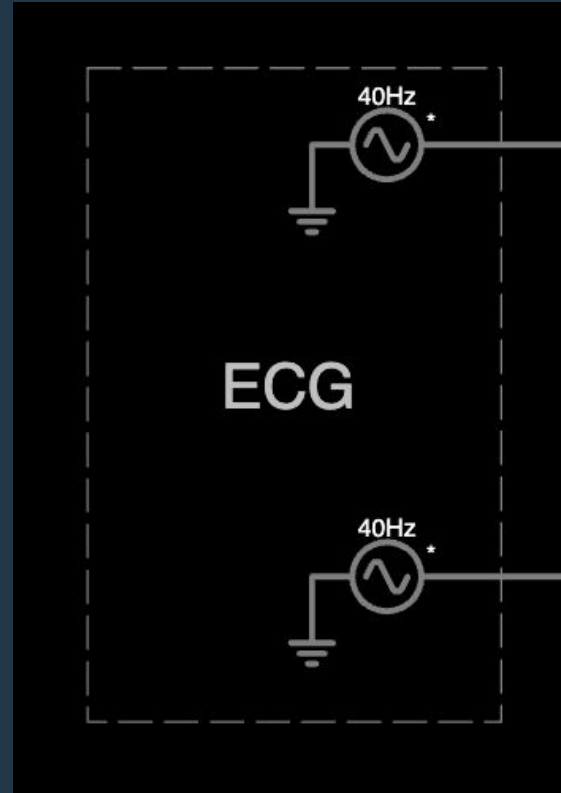


The image features a dark blue background with a decorative border of hand-drawn medical icons. The top border includes syringes, pills, and stethoscopes in red, teal, and white. The bottom border features band-aids, pills, and stethoscopes in white, red, and teal. The central text 'Part II Analysis' is written in a white, casual script font.

Part II Analysis

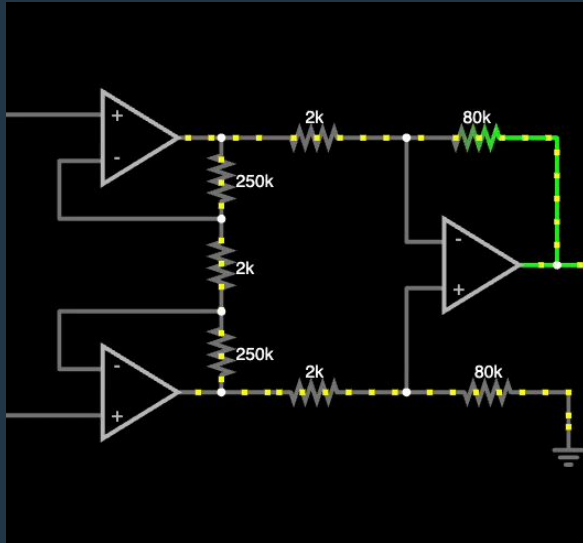
ECG sensor inputs

- Takes input voltage from biopotential amplifier and feeds a 40 Hz sinusoidal waveform into the circuit
- Simulating true ECG voltage output values
 - Top source = 2.5mV
 - Bottom source = 3mV



Instrumentation Amplifier

- Waveforms from the biopotential signal goes through the amplifier to improve signal quality to reduce noise-level.
- Voltage out of the amplifier is 10000 times the input voltage



$$Ad = \left| \left(1 + 2 * \frac{R_o}{R_a} \right) * \left(-\frac{R_4}{R_3} \right) \right| = 10,000$$

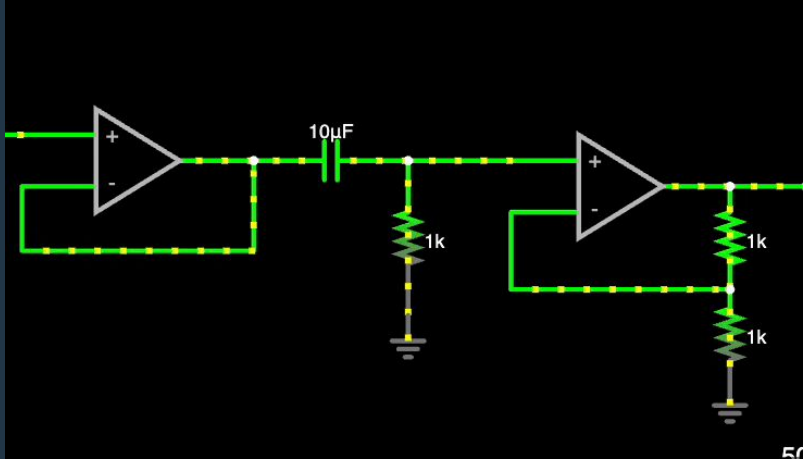
$$R_o = 249 \text{ k}\Omega$$

$$R_o = R_3 = 2 \text{ k}\Omega$$

$$R_4 = 80 \text{ k}\Omega$$

Buffer #2 and Passive RC High Pass Filter

- Passive RC high pass filter
 - Allows signals with high frequencies to pass through
- Isolates the previous and the next stages of the circuit so that they do not affect each other.



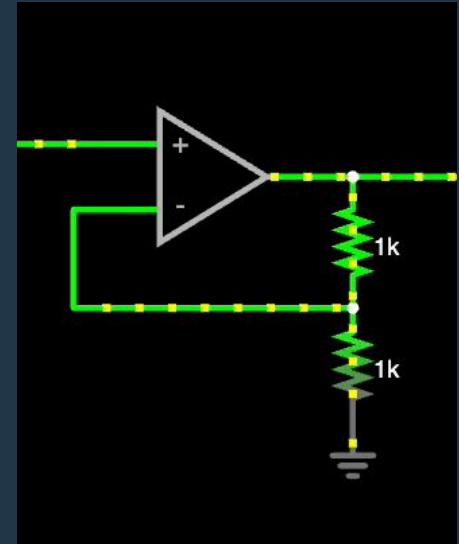
$$C_1 = 10\mu\text{F}$$
$$R_1 = R_2 = R_3 = 1\text{k}\Omega$$

Comparator #2

- Signal from the high pass filter connects to the inverting input of the comparator
- Considerations: regular ECG peak voltages: 2.5~3 mV
- Compare our input ECG R wave peak voltages with the regular ECG.
- If $V_{in} < V_{ref}$, $V_{out} = V_{+}$
- If $V_{in} > V_{ref}$, $V_{out} = V_{-}$
- $V_{ref} = 3V$, $V_{+} = 5V$, $V_{-} = GND$

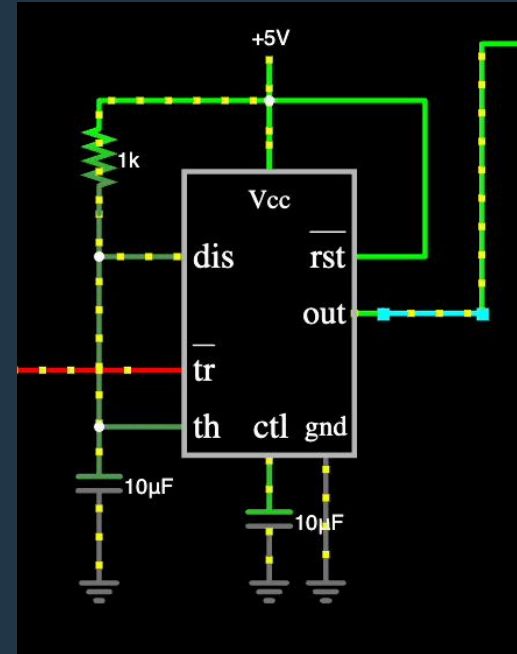
$$R_{ref,GND} = 2k\Omega$$

$$R_{ref,out} = 3k\Omega$$



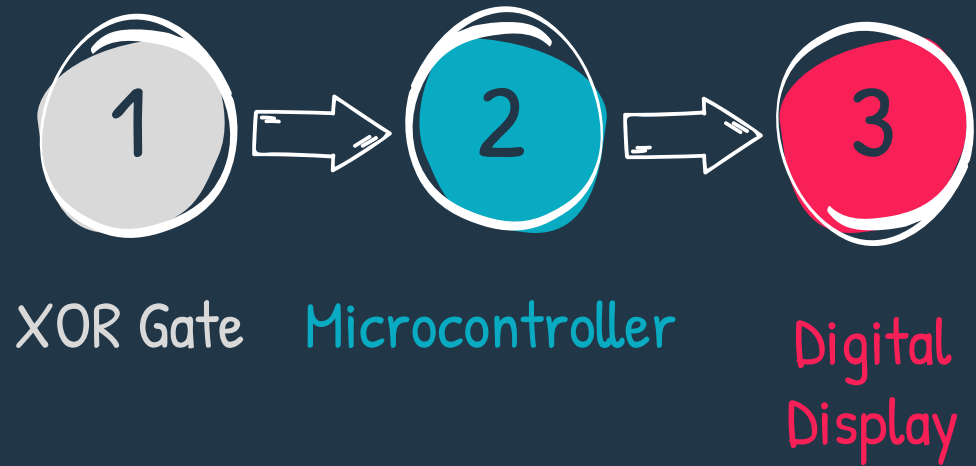
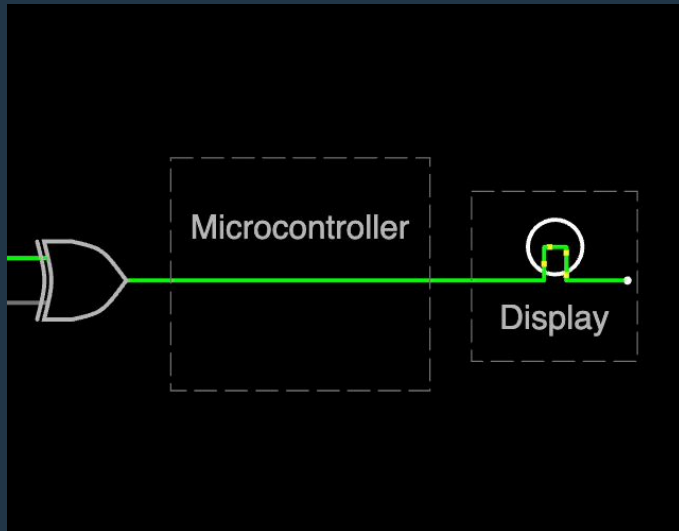
555 Monostable Timer #2 (ECG)

- Timer #2 activates when it receives a voltage signal from comparator 2.
- Once activated, output stays high for time interval $T = RC\ln(3)$
- Time interval selected based on ECG properties: $T = 600\text{ms}$
- One set of RC values: $R = 546\text{ k}\Omega$, $C = 1\mu\text{F}$



Part III: XOR, Microcontroller, & Display

Overall Goal: develop measured pulse transit time and compare value to detect abnormal BP and display warning messages.



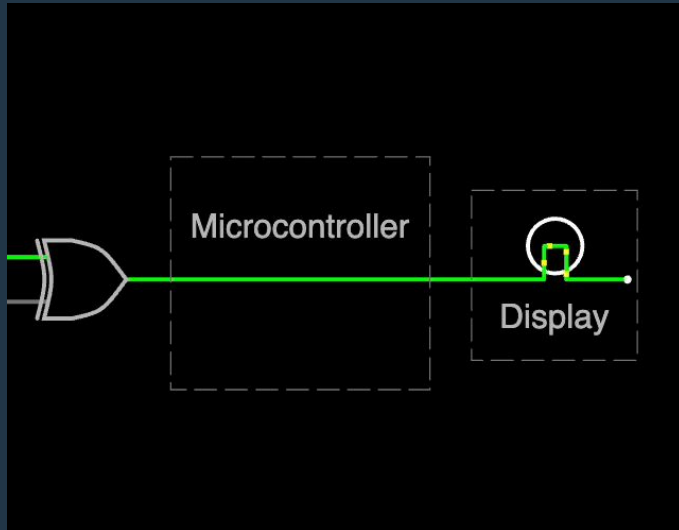


Part III Analysis



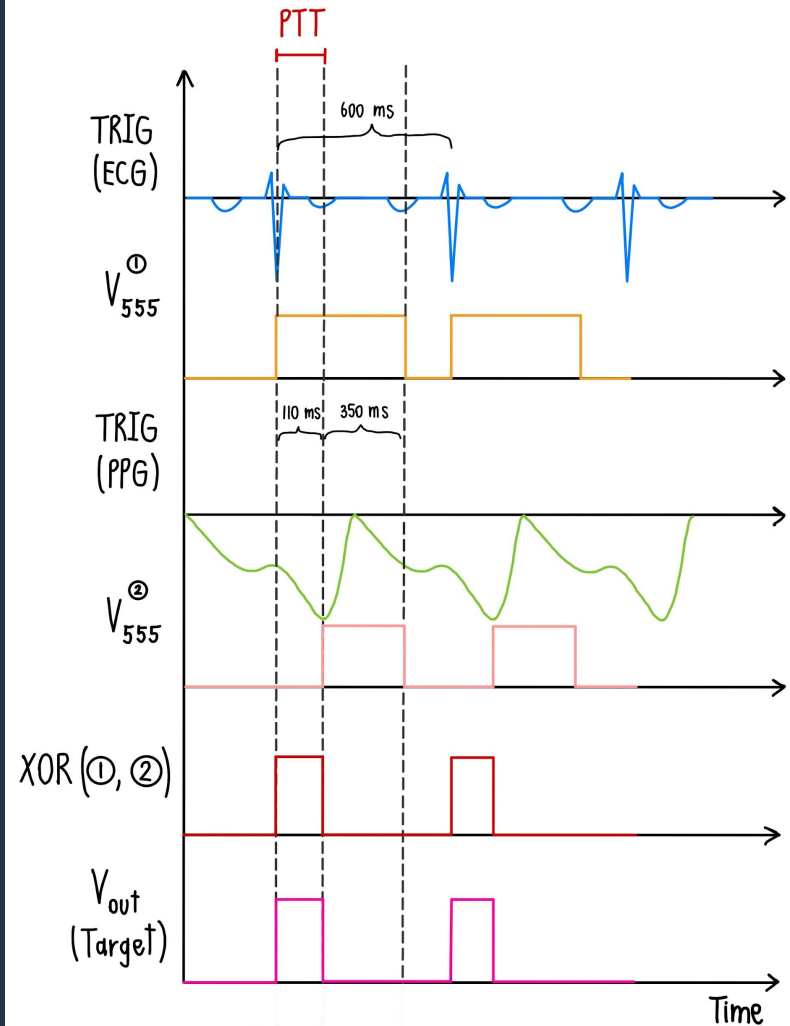
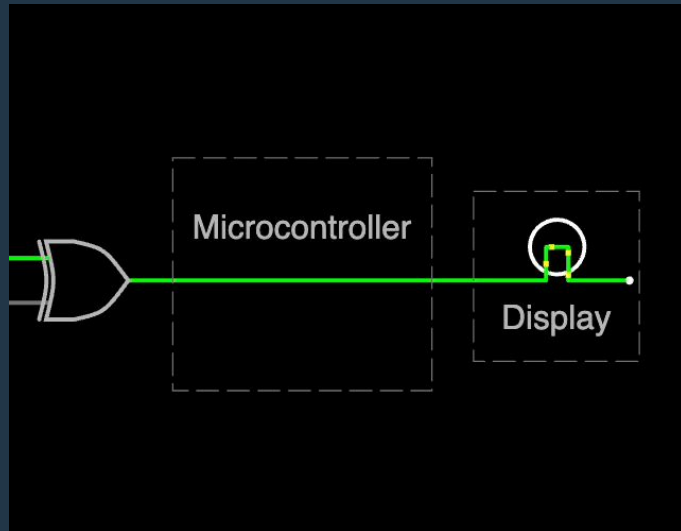
XOR Gate

- Takes input from the two timers.
- XOR gate produces a TRUE output if the two timers are not sending out outputs concurrently
 - The TRUE message feeds into the microcontroller.



Timer 1(A)	Timer 2(B)	OUT
0	0	0
0	1	1
1	0	1
1	1	0

V_{in} of the timers vs V_{out} of the
timers vs XOR gate responses



Microcontroller & Digital display

- Takes voltage output from XOR gate
 - Includes built-in code that calculates amount of time the XOR gate was activated → that time is the PTT
 - Uses equation below to convert PTT to BP
- Converts analog signal containing BP information to digital as it leads into a digital display.
- The digital display will show the BP and a warning message if microcontroller determines that the BP is higher than 140 mmHg.

$$BP = \frac{\Delta BP}{0.7} = \frac{1}{0.7} \left(\frac{1}{2} \rho \frac{d^2}{PTT^2} + \rho gh \right) = \frac{A}{PTT^2} + B$$

$$A = (0.48 \times height)^2 \times \frac{\rho}{1.4}$$

Design Limitations

- Currently inaccurate compared to traditional cuff-based blood pressure readings
- Vulnerable to physiological, environmental, and motion-induced noise
 - Due to changes in heart-wrist length, there may be fluctuations in blood pressure readings
- Necessitates regular calibrations for reliable readings
- ECG leads must be constantly worn to operate
 - Product limited to medical settings
 - Potential future consideration

Significance and potential applications

- Enables long-term tracking and data collection for inpatient blood pressure monitoring
- Widespread applicability to diagnosing blood pressure related medical conditions



Acknowledgements

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